

1 **M1 disruption delays motor processes but not deliberation about**  
2 **action choices**

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4 Gerard Derosiere<sup>1</sup>, David Thura<sup>2</sup>, Paul Cisek<sup>3</sup>, Julie Duque<sup>1</sup>

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7 <sup>1</sup> *Institute of Neuroscience, Laboratory of Neurophysiology, Université catholique de*  
8 *Louvain, Brussels, Belgium*

9  
10 <sup>2</sup> *Lyon Neuroscience Research Center - Impact team, Inserm U1028 - CNRS UMR 5292,*  
11 *Bron, France*

12  
13 <sup>3</sup> *Department of Neuroscience, Université de Montréal, Montréal, QC H3T 1J4, Canada*  
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18 Corresponding author contact details:

19 **Gerard Derosiere**

20 CoActions Lab

21 Institute of Neuroscience

22 Université catholique Louvain

23 Av. Mounier, 53 - Bte B1.53.04

24 1200 Bruxelles, Belgium

25 Tel: + 32 (0)2 764 54 20

26 Email address: [gerard.derosiere@uclouvain.be](mailto:gerard.derosiere@uclouvain.be)

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29 Running title: “M1 disruption and motor decisions”

30 **Abstract**

31 Decisions about actions typically involve a period of deliberation that ends with the  
32 commitment to a choice and the motor processes overtly expressing that choice. Previous  
33 studies have shown that neural activity in sensorimotor areas, including the primary motor  
34 cortex (M1), correlates with deliberation features during action selection. Yet, the causal  
35 contribution of these areas to the decision process remains unclear. Here, we investigated  
36 whether M1 determines choice commitment, or whether it simply reflects decision signals  
37 coming from upstream structures and instead mainly contributes to the motor processes that  
38 follow commitment. To do so, we tested the impact of a disruption of M1 activity, induced by  
39 continuous theta burst stimulation (cTBS), on the behavior of human subjects in (1) a simple  
40 reaction time (SRT) task allowing us to estimate the duration of the motor processes and (2) a  
41 modified version of the tokens task (Cisek et al., 2009), which allowed us to estimate  
42 subjects' time of commitment as well as accuracy criterion. The efficiency of cTBS was  
43 attested by a reduction in motor evoked potential amplitudes following M1 disruption, as  
44 compared to those following a sham stimulation. Furthermore, M1 cTBS lengthened SRTs,  
45 indicating that motor processes were perturbed by the intervention. Importantly, all of the  
46 behavioral results in the tokens task were similar following M1 disruption and sham  
47 stimulation, suggesting that the contribution of M1 to the deliberation process is potentially  
48 negligible. Taken together, these findings favor the view that M1 contribution is downstream  
49 of the decision process.

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55 **New and noteworthy**

56 Decisions between actions are ubiquitous in the animal realm. Deliberation during action  
57 choices entails changes in the activity of the sensorimotor areas controlling those actions, but  
58 the causal role of these areas is still often debated. Using continuous theta burst stimulation,  
59 we show that disrupting the primary motor cortex (M1) delays the motor processes that follow  
60 instructed commitment but does not alter volitional deliberation, suggesting that M1  
61 contribution may be downstream of the decision process.

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63 **Key-words**

64 Motor cortex, TMS, urgency, action selection, movement preparation

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77 **INTRODUCTION**

78       The physical world provides animals with a variety of action opportunities, constantly  
79 requiring them to make decisions, some of which are critical for survival. For instance, the  
80 choice of a car driver to turn left or right in front of a sudden obstacle may have dramatic  
81 consequences on her/his life and on that of the pedestrians around. The driver will have to  
82 quickly deliberate and commit to one action.

83       Deliberation about actions is thought to entail a competition between distinct neural  
84 populations within the motor system (Pezzulo and Cisek, 2016; Svoboda and Li, 2018). In  
85 this view, separate action opportunities increase activity of distinct populations, which  
86 compete against each other, possibly through mutual inhibition (Michelet et al., 2010). An  
87 action is eventually selected and executed when activity in the related population reaches a  
88 critical decision threshold (Laming, 1968; Ratcliff, 1978; Stone, 1960).

89       In line with this hypothesis, a compendium of studies has shown that the dorsal premotor  
90 (PMd), but also the primary motor cortex (M1), display a buildup of choice-selective activity  
91 during the decision process. The rate of this buildup depends on the amount of sensory  
92 evidence favoring the selection of each action in the environment (Alamia et al., 2018;  
93 Derosiere et al., 2018; Donner et al., 2009; Gould et al., 2012; Tosoni et al., 2014; Wyart et  
94 al., 2012). According to this view, in the car driver example above, the presence of  
95 pedestrians on the right side of the street would increase the activity of the population coding  
96 for the movement of rotating the wheel towards the left, and possibly weaken the activity of  
97 the population favoring the opposite rightward rotation movement. Ultimately, the driver will  
98 commit to turning left and execute the related action, to avoid hitting the group of people.

99           Importantly, making decisions often requires balancing the desire to take time to  
100 deliberate accurately (*i.e.*, to accumulate sensory evidence and make the best choice) with the  
101 urge to act (Churchland et al., 2008; Forstmann et al., 2008; Hanks et al., 2011; Thura and  
102 Cisek, 2014a). During a speeded decision, the urge to act increases as time passes (Cisek et  
103 al., 2009, Ditterich, 2006, Drugowitsch et al., 2012, Seideman et al., 2018; Thura et al., 2012)  
104 but the overall level of urgency also varies depending on the context (Murphy et al., 2016,  
105 Thura et al., 2014; Thura and Cisek, 2016, 2017). In the situation described earlier, the  
106 driver's level of urgency will be higher if the obstacle suddenly appears close to the car than if  
107 it appears far away. As evident in this example, adjustments in urgency alter the balance  
108 between decision speed and accuracy – *i.e.*, the so-called speed-accuracy tradeoff: choices are  
109 more likely to be incorrect when time pressure is elevated, while accuracy improves when  
110 temporal demands permit long deliberation (*e.g.*, Hanks et al., 2011; Seideman et al., 2018).

111           At the neural level, several lines of evidence indicate that higher levels of urgency during  
112 deliberation about action choices modulate neural activity in PMd and M1 (Murphy et al.,  
113 2016; Steinemann et al., 2018, Thura and Cisek, 2014a, 2016). In these areas, activity is  
114 globally amplified at baseline and then builds-up at a faster rate when urgency is high  
115 compared to when it is low, reducing the time needed to reach decision threshold but at the  
116 cost of accuracy (Thura and Cisek, 2016). Recent findings suggest that the basal ganglia  
117 (Thura and Cisek, 2017; van Maanen et al., 2016) and the locus coeruleus (Hauser et al.,  
118 2018; Murphy et al., 2016) may contribute to generate such a modulation of motor cortical  
119 activity.

120           Together, these data indicate that the motor cortical areas combine both the sensory  
121 evidence signals guiding the choice with the urgency-related signals determining the best time  
122 to commit to that choice, suggesting a crucial role of these areas in the decision-making  
123 process. To date, however, a causal test of this role is lacking.

124 Here, we investigated whether M1 causally contributes to deliberation about action  
125 choices, or whether it simply reflects decision signals coming from upstream areas, such as  
126 PMd, the basal ganglia, or the locus coeruleus. It has previously been shown that disrupting  
127 M1 activity by means of continuous theta burst stimulation (cTBS) causes finger responses to  
128 slow down (Huang et al., 2005; Lakhani et al., 2014; McAllister et al., 2013). However, it is a  
129 matter of debate whether this effect should be interpreted as a slowing down of processes  
130 involved in deciding which action to perform (*i.e.*, in the deliberation process) or as a slowing  
131 down of the motor processes that follow commitment (*i.e.*, of movement initiation and  
132 execution). In fact, a slowing down of the deliberation process has been associated with  
133 reduced urgency during volitional decision behavior (Hanks et al., 2011; Seideman et al.,  
134 2018; Thura and Cisek, 2014a, 2016). If M1 is causally involved in the decision process, then  
135 M1 disruption might lengthen deliberation in a manner consistent with reduced urgency as  
136 compared to a sham cTBS session. Conversely, if M1 is mainly involved in initiating and  
137 executing selected actions, then its disruption should have no effect on the deliberation  
138 portion of response time, and should only slow down the motor processes that follow  
139 commitment to an action. These hypotheses were tested by characterizing action choices in a  
140 modified version of the tokens task (Cisek et al., 2009), which is specifically designed to  
141 estimate subjects' time of commitment, their accuracy criterion and infer from those variables  
142 their urgency functions (Thura et al., 2014a).

143

## 144 **MATERIALS AND METHODS**

### 145 **Participants**

146 19 healthy right-handed subjects participated in this study (10 women;  $24 \pm 3.5$  years  
147 old). Participants were financially compensated for their participation and earned additional

148 money depending on their performance in a decision-making task (see *Task* section below).  
149 The protocol was approved by the institutional review board of the catholic University of  
150 Louvain (UCLouvain), Brussels, Belgium, and required written informed consent, in  
151 compliance with the principles of the Declaration of Helsinki.

152

### 153 **Experimental design**

154 Experiments were conducted in a quiet and dimly-lit room. Subjects were seated at a  
155 table in front of a 21-inch cathode ray tube computer screen. The display was gamma-  
156 corrected and its refresh rate was set at 100 Hz. The computer screen was positioned at a  
157 distance of 70 cm from the subject's eyes and was used to display stimuli during the decision-  
158 making task. Left and right forearms were rested upon the surface of the table with the palms  
159 facing the table. A computer keyboard was positioned upside-down under the dominant (*i.e.*,  
160 right) hand with the response keys F9 and F8 under the index and middle fingers, respectively  
161 (see Figure 1).

162

### 163 **Task**

164 The task used in the current study is a variant of the “tokens task” (Cisek et al., 2009) and  
165 was implemented by means of LabView 8.2 (National Instruments, Austin, TX). The  
166 sequence of events in each trial is depicted in Figure 1. Between trials, subjects were always  
167 presented with a default screen consisting of three circles (4.5 cm diameter), displayed for  
168 2000 ms on a white background. Fifteen randomly arranged tokens (0.3 cm diameter) then  
169 appeared in the central circle. After a delay of 800 ms, the tokens began to jump, one-by-one  
170 every 200 ms from the center to one of the two lateral circles (*i.e.*, Jump<sub>1</sub> to Jump<sub>15</sub>). The  
171 subjects' task was to indicate by a right index or right middle finger key-press which lateral

172 circle they thought would ultimately receive the majority of the tokens (*i.e.*, F9 and F8 key-  
173 presses to choose left and right circles, respectively). They could provide their response as  
174 soon as they felt sufficiently confident, but between Jump<sub>1</sub> and Jump<sub>15</sub>. Once the response  
175 was provided, the tokens kept on jumping every 200 ms until the central circle was empty. At  
176 this time, the selected circle was highlighted either in green or in red depending on whether  
177 the response was correct or incorrect, respectively, and a score was displayed above the  
178 central circle to provide the subjects with further feedback of their performance. In correct  
179 trials, subjects received a positive score (*i.e.*, a monetary reward) which was equal to the  
180 number of tokens remaining in the central circle at the time of the response (in € cents).  
181 Conversely, incorrect responses led to a fixed penalty of 7 cents, regardless of the RT. Thus,  
182 the longer the subjects waited to provide a response, the lower was the reward/penalty ratio,  
183 generating an increasing sense of urgency as time passed within each trial. In the absence of  
184 any response before Jump<sub>15</sub>, the central circle was highlighted in red and a “Time Out” (TO)  
185 message appeared on the top of the screen. The subjects were neither rewarded nor penalized  
186 in these trials. The feedback cue remained on the screen for 1000 ms and then disappeared at  
187 the same time as the tokens did, denoting the end of the trial. Subjects were told that they  
188 would receive a monetary reward at the end of the experiment corresponding to their final  
189 score. Each trial lasted 6600 ms.

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192

### 193 **Blocks and sessions**

194 The study included 3 sessions, conducted on separate days at a 24-hour interval. Testing  
195 always occurred at the same time of the day for a given subject, to avoid variations that could



196 be due to changes in chronobiologic states (Derosiere et al., 2015a; Schmidt et al., 2006).  
197 Each session comprised 4 blocks of 50 trials, with each block lasting about 5.5 minutes.  
198 Subjects also performed 4 blocks of 5 trials of a simple reaction time (SRT) task, two at the  
199 beginning and two at the end of each session. In the SRT task, subjects were presented with  
200 the same display as in the tokens task described above. However, after 50 ms in the central  
201 circle, the 15 tokens all jumped together into one of the two lateral circles at the same time.  
202 Subjects were instructed to respond to this “GO signal” by pressing the corresponding key as  
203 fast as possible. Importantly, the 15 tokens always jumped into the same lateral circle in all  
204 trials of a given SRT block and subjects were told which lateral circle this would be in  
205 advance. This SRT task allowed us to estimate the sum of the delays attributable to the  
206 sensory and motor processes in the absence of a choice (see Cisek et al., 2009; Thura et al.,  
207 2014).

208 Day 1 served as a training session. Day 2 and 3 corresponded to the actual experimental  
209 sessions with the cTBS intervention (Figure 2). cTBS was applied before subjects engaged in  
210 the blocks of trials, either over the left M1 hand area (M1-Disruption session) or over the right  
211 primary somatosensory cortex (S1), 2 cm behind the right M1 area (Sham session; Derosiere  
212 et al., 2014; Alexandre et al., 2015; Torta et al., 2013), in a randomized order. The Sham  
213 session allowed us to ensure that the putative behavioral effects observed following M1 cTBS  
214 were not due to the tactile and auditory sensations elicited by the TMS pulses (Derosiere et  
215 al., 2017a, 2017b).

216

## 217 **TMS procedure**

218 TMS was delivered through a 2x75 mm figure-of-eight coil connected to a Magpro X100  
219 Stimulator (Magventure Company, Farum, Denmark). The coil was placed tangentially on the

220 scalp with the handle oriented towards the back of the head and laterally at a 45° angle away  
221 from the midline. At the beginning of each session, the M1 hand area was localized by  
222 identifying the optimal spot (called the “hotspot”) for eliciting MEPs in the first dorsal  
223 interosseous (FDI) muscle of the right hand (M1-Disruption session) or the left hand (Sham  
224 session). To do so, we relied on markers disposed on an electroencephalography (EEG) cap  
225 fitted on the participant’s head (Duque et al., 2010, 2014; Vandermeeren et al., 2009). We  
226 first applied the stimulation with the center of the coil over the C3 or C4 location of the EEG  
227 cap (*i.e.*, corresponding to the right and left M1 areas, respectively). Stimulation intensity was  
228 increased until obtaining consistent MEP responses at this location. We then moved the coil  
229 by steps of approximately 0.5 cm around this location both in the rostro-caudal and in the  
230 medio-lateral axis. Stimulation was applied with the previously defined intensity at each new  
231 location and MEP amplitudes were visually screened. The hotspot was defined as the location  
232 at which the largest and most consistent MEP amplitudes could be obtained. The coil was  
233 then held at this location and the edges of its shape were marked on tapes disposed on the  
234 EEG cap. These marks allowed us to localize the hotspot at any required time during the  
235 session. Once the hotspot was found, we determined the resting motor threshold (rMT). The  
236 rMT was defined as the minimal intensity required to evoke MEPs of 50  $\mu$ V peak-to-peak in  
237 the targeted muscle on 5 out of 10 consecutive trials at the hotspot (Grandjean et al., 2018;  
238 Rothwell et al., 1991; Rossini et al., 1994, 2015; Vassiliadis et al., 2018).

239 The cTBS procedure consisted of a series of short TMS trains (three pulses at 50 Hz)  
240 repeated every 200 ms for a total duration of 40 s (600 pulses) at an intensity of 80 % of rMT  
241 (Derosiere et al., 2017a, 2017b; Huang et al., 2005; Solopchuk et al., 2017). Such an  
242 intervention has been shown to inhibit the stimulated cortical area, producing a temporary  
243 “virtual lesion”, often effective as soon as the train is over (Derosiere et al 2017a, 2017b; Do

244 et al., 2018; Sasaki et al. 2018) and lasting for between 20 (Clerget et al., 2011; Oberman et  
245 al., 2011; Zénon et al., 2015) and 45 minutes (Huang et al., 2005).

246 In order to monitor the inhibitory effect of cTBS on motor activity, single TMS pulses  
247 were applied at the M1 hotspot at 115 % of the rMT to elicit MEPs at different time points in  
248 the M1-Disruption and Sham sessions (Klein et al., 2014; Labruna et al., 2014; Quoilin et al.,  
249 2016, 2017). In the M1-Disruption session, MEPs were recorded in the right FDI following  
250 TMS over left M1, to evaluate the impact of left M1 cTBS on left motor excitability. In the  
251 Sham session, MEPs were obtained from the left FDI following TMS over right M1, to  
252 control for the absence of effect of right S1 cTBS on right M1 excitability.

253 The time points at which MEPs were elicited in the M1-Disruption and Sham sessions  
254 were comparable (see Figure 2). In both sessions, 20 MEPs were elicited at the beginning of  
255 the session (*i.e.*, just before cTBS; TMS<sub>Baseline</sub>). Then, 15 MEPs were elicited just following  
256 cTBS (TMS<sub>1</sub>), after the two initial SRT blocks (TMS<sub>2</sub>), and after each block of trials of the  
257 tokens task (TMS<sub>3-6</sub>). Finally, 20 additional MEPs were evoked following the two last SRT  
258 blocks (TMS<sub>7</sub>). These seven timings (TMS<sub>1-7</sub>) fell 1 min, 3 min, 11 min, 19 min, 27 min, 35  
259 min, and 37 min after the cTBS intervention, respectively.

260

## 261 **Data collection**

262 Electromyography (EMG) was used to measure the peak-to-peak amplitude of FDI MEPs  
263 elicited by single TMS pulses over the contralateral M1. EMG activity was recorded from  
264 surface electrodes placed over the right FDI or the left FDI (M1-Disruption or Sham sessions,  
265 respectively). EMG data were collected for 1000 ms on each trial, starting 300 ms before the  
266 TMS pulse. EMG signals were amplified, bandpass filtered on-line (10-500 Hz) and digitized  
267 at 2000 Hz for off-line analysis.

268

## 269 **Data analysis**

### 270 *Motor evoked potential data*

271 MEP data were collected with Signal (Signal 3.0, Cambridge, UK) and analyzed with  
272 custom Signal scripts. MEP amplitudes were measured for each TMS pulse. Trials with  
273 background EMG activity greater than 20  $\mu\text{V}$  on average (root mean square, rms), in the 200-  
274 ms window preceding the TMS artifact, were excluded from the analysis.  $3.63 \pm 5.43$  % of  
275 trials were discarded based on this criterion. The amplitude of MEPs elicited at each time  
276 point was averaged to obtain a measure of motor excitability at  $\text{TMS}_{\text{Baseline}}$  and at  $\text{TMS}_{1-7}$   
277 the M1-Disruption and Sham sessions (Figure 2). For each session, we then expressed MEP  
278 amplitudes obtained at  $\text{TMS}_{1-7}$  (*i.e.*, after the cTBS intervention) in percentage of the  
279 amplitudes measured at  $\text{TMS}_{\text{Baseline}}$  (*i.e.*, before the cTBS intervention).

280 The disruptive impact of cTBS on cortical activity varies between subjects (Do et al.,  
281 2018; Jannati et al., 2017; Rocchi et al., 2018). Here, we aimed at only including individuals  
282 in which cTBS effectively disrupted M1. To do so, we discarded subjects presenting  
283 percentage MEP amplitudes exceeding 2.5 SD *above* the mean of the group in the M1-  
284 disruption session at one of the  $\text{TMS}_{\text{EPOCHS}}$  or more. This led to the rejection of three subjects,  
285 who exhibited average MEP amplitudes of  $148.3 \pm 12.5$  %,  $139.5 \pm 10.6$  % and  $188.6 \pm$   
286  $20.9$ % following the cTBS intervention in the M1-disruption session (all  $\text{TMS}_{\text{EPOCHS}}$  averaged  
287 together), reflecting thus a large increase (rather than the targeted decrease) in motor  
288 excitability. The analyses of the MEP and behavioral data were performed on the remaining  
289 pool of subjects ( $n = 16$ ).

290

### 291 *Behavioral data*

292 Behavioral data were collected with LabVIEW 8.2 (National Instruments, Austin, TX),  
293 stored in a database (Microsoft SQL Server 2005, Redmond, WA), and analyzed with custom  
294 MATLAB scripts (MathWorks, Natick, MA). Because Day 1 served as a training session (see  
295 section *Blocks and sessions*), the behavioral analyses focused on the data acquired on Day 2  
296 and 3 (*i.e.*, in the M1-Disruption and Sham sessions).

297

### 298 *SRT task*

299 For each subject, we computed the mean SRT for both fingers (right index and right  
300 middle fingers), defined as the difference between the time at which subjects pressed the key  
301 and the time at which the 15 tokens appeared simultaneously in the lateral circle, obtained at  
302 the beginning (SRT<sub>1</sub>) and at the end (SRT<sub>2</sub>) of each session. This SRT allowed us to quantify  
303 the impact of M1 cTBS on the motor processes that follow commitment to an action in the  
304 absence of a choice.

305

### 306 *Tokens task*

#### 307 Classification of the trial types based on the temporal profile of the success probability

308 The task allows us to calculate, at each moment in time, the “success probability”  $p_i(t)$   
309 associated with choosing each lateral circle  $i$ . For a total of 15 tokens, if at a particular  
310 moment in time the right (R) circle contains  $N_R$  tokens, the left (L) circle contains  $N_L$  tokens,  
311 and the central (C) circle contains  $N_C$  tokens, then the probability that the circle on the right  
312 will ultimately be the correct one is described as follows:

$$p(R|N_R, N_L, N_C) = N \frac{N_C!}{2^{N_C}} \sum_{k=0}^{\min(N_C, 7-N_L)} \frac{1}{k! (N_C - k)!}$$

313

(1)

314 For some of the analyses, we grouped trials according to the temporal profile of  $p_i(t)$ .  
315 That is, although the side of each token jump was completely random in each trial, we could  
316 classify some trials as belonging to one of two specific types a posteriori. Trials were  
317 categorized as “obvious” when the  $p_i(t)$  was above 0.6 after Jump<sub>2</sub> and above 0.75 after  
318 Jump<sub>5</sub>; that is, the initial token jumps consistently favored the correct circle. Other trials were  
319 categorized as “ambiguous” when the initial jumps were balanced between the lateral circles,  
320 keeping the  $p_i(t)$  close to 0.5 until late in the trial:  $p_i(t)$  remained between 0.5 and 0.66 up to  
321 Jump<sub>7</sub> in these trials.

322

323 Decision Time (DT), percentage of correct choices (%Correct) and percentage of time out  
324 trials (%TO)

325 For each session (M1-Disruption and Sham) and each trial type (obvious and ambiguous;  
326 trials that were neither obvious nor ambiguous were not considered here), we analyzed the  
327 following behavioral variables: the decision time (DT), the percentage of correct choices  
328 (%Correct) and the percentage of time out trials (%TO). To evaluate the DT, we first  
329 calculated the RT during the tokens task by computing the difference between the time at  
330 which subjects pressed the key and Jump<sub>1</sub>. We then subtracted from this tokens RT, the mean  
331 RT obtained in the SRT task on the same day (SRT<sub>1</sub> and SRT<sub>2</sub> pooled together), providing us  
332 with an estimate of DT, reflecting the duration of the deliberation process for each subject.  
333 Note that we used a monetary reward in the tokens but not in the SRT task, which might have  
334 led us to slightly underestimate the DT. That is, previous studies have shown that monetary  
335 reward can boost motor processes (Reppert et al., 2018; Summerside et al., 2018; Yoon et al.,  
336 2018). Hence, the latter might have been faster in the tokens than in the SRT task used to

337 estimate it. Thus, we might have subtracted a too large value from the tokens RT, shortening  
338 the DT. Still, this putative underestimation of DT applies for both the M1-disruption and the  
339 Sham sessions and has thus no biasing impact on our data.

340

#### 341 Sensory evidence at decision time (DT)

342 Sensory evidence refers to the available information supporting the correct choice. In the  
343 tokens task, the sensory evidence is determined by the difference between the number of  
344 tokens in each lateral circle; the more the correct circle contains a large number of tokens,  
345 compared to the other lateral circle, the higher the evidence. Given that tokens jump one by  
346 one in this task, sensory evidence changes after each jump. We can estimate the evidence  
347 based on which subjects made their decision by computing after each jump a first-order  
348 approximation of the real probability function (equation 1), called the sum of log-likelihood  
349 ratios (SumLogLR), and then compute this quantity at decision time (Cisek et al., 2009):

$$SumLogLR(n) = \sum_{k=1}^n \log \frac{p(e_k|S)}{p(e_k|U)}$$

350 (2)

351 In this equation,  $p(e_k|S)$  is the likelihood of a token event  $e_k$  (a token jumping into either  
352 the selected or unselected lateral circle) during trials in which the selected lateral circle  $S$  is  
353 correct and  $p(e_k|U)$  is the likelihood of  $e_k$  during trials in which the unselected circle  $U$  is  
354 correct. The SumLogLR is proportional to the difference between the number of tokens that  
355 moved towards each lateral circle before the decision. Hence, the lower the amount of sensory  
356 evidence in favor of the chosen lateral circle, the lower the SumLogLR.

357 To characterize the decision policy of the subjects in the Sham and M1-Disruption  
358 sessions, we determined the level of sensory evidence at the time of commitment (*i.e.*, at DT).

359 To do so, we binned trials as a function of the total number of tokens that moved before the  
360 decision, and calculated the average SumLogLR for each bin as performed in previous studies  
361 exploiting the tokens task (*e.g.*, Thura and Cisek, 2014, 2017). Seven bins were defined, with  
362 the first bin (Bin<sub>1</sub>) including responses provided between Jump<sub>5</sub> and Jump<sub>6</sub>, the second bin  
363 (Bin<sub>2</sub>) including responses provided between Jump<sub>6</sub> and Jump<sub>7</sub> and so on, until the last bin  
364 (Bin<sub>7</sub>) covering the period between Jump<sub>11</sub> and Jump<sub>12</sub>. SumLogLR at DT preceding Jump<sub>5</sub> or  
365 following Jump<sub>12</sub> were not considered for this analysis because part of the subjects did not  
366 respond at these timings. Importantly, the SumLogLR at DT was computed based on every  
367 trial where a response was provided (*i.e.*, for correct and incorrect responses, in obvious and  
368 ambiguous trials, as well as in other trials with different  $p_i(t)$ ).

369

### 370 Estimation of urgency functions

371 According to recent models of decision-making, action choices result from the  
372 combination of signals that track the available sensory evidence and the level of urgency that  
373 grows over time (Cisek et al., 2009, Ditterich, 2006, Drugowitsch et al., 2012). For instance,  
374 in a minimal implementation of the urgency gating model (Cisek et al., 2009; Thura et al.,  
375 2012), evidence is multiplied by a linearly increasing urgency signal, and then compared with  
376 a threshold. The result can be expressed as follows:

$$y_i = (N_i - N_{j \neq i}) \cdot [mt + b]^+ < T$$

377 (3)

378 where  $y_i$  is the “neural activity” for choices to target  $i$ ,  $N_i$  is the number of tokens in target  $i$ ,  $t$   
379 is the number of seconds elapsed since the start of the trial,  $m$  and  $b$  are the slope and y-  
380 intercept of the urgency signal, and  $[ ]^+$  denotes half-wave rectification (which sets all  
381 negative values to zero). When  $y_i$  for any target crosses the threshold  $T$ , that target is chosen.



382 A direct prediction of such urgency-based models is that decisions made with low levels  
383 of evidence should be associated with high levels of urgency, and vice-versa. That is, one core  
384 assumption is that a high urgency should push one to commit to a choice even if evidence for  
385 that choice is weak. Hence, the SumLogLR at DT values (*i.e.*, reflecting the available sensory  
386 evidence at the time of commitment in the tokens task) can be exploited to estimate the level  
387 of urgency at DT. Here, we first multiplied the SumLogLR at DT values by -1 (*i.e.*, to  
388 “rectify” them; please see Figure 3), given the theoretical inverse relationship between  
389 sensory evidence and urgency at DT. We then added a constant of 3 to the rectified curves to  
390 obtain positive urgency values. Finally, we fitted a linear regression over the rectified positive  
391 values. We extracted the intercept and the slope of these so-called urgency functions, which  
392 we used as estimates of the initial level and the growth rate of the urgency signal,  
393 respectively. Second-order polynomial regressions were also performed on the rectified  
394 SumLogLR data but did not yield significantly better fits (*i.e.*, group-level Bayesian  
395 Information Criterion [BIC] values for linear and polynomial fits were  $5.75 \pm 1.61$  and  $5.74 \pm$   
396  $1.79$  a.u., respectively;  $t_{14} = 0.02$ ,  $p = .984$ ).

397

398

### 399 **Statistical analysis**

400 All statistical analyses were performed with custom R Scripts (R Version 3.4.1, Car and  
401 BayesFactor packages). All data were examined for normality and homogeneity of variance  
402 using Skewness, Kurtosis and Brown-Forsythe tests. The significance level for all tests was  
403 set at  $p < .05$ , except when Bonferroni corrections were applied. All results are expressed as  
404 mean  $\pm$  SE.

405

406 ***Motor evoked potential data***

407 MEP data (expressed in percentage of MEPs at TMS<sub>Baseline</sub>) were analyzed using a two-  
408 way repeated-measure ANOVA (ANOVA<sub>RM</sub>) with SESSION (M1-Disruption, Sham) and  
409 TMS<sub>EPOCH</sub> (TMS<sub>1</sub>, TMS<sub>2</sub>, TMS<sub>3</sub>, TMS<sub>4</sub>, TMS<sub>5</sub>, TMS<sub>6</sub>, TMS<sub>7</sub>) as within-subject factors.  
410 Moreover, the percentage MEP values obtained for each TMS<sub>EPOCH</sub> were compared against  
411 100 % using Bonferroni-corrected single-sample Student's t-tests to identify any significant  
412 suppression in the M1-Disruption and in the Sham session.

413

414 ***Behavioral data***

415 The SRT data were analyzed using a two-way ANOVA<sub>RM</sub> with SESSION (M1-  
416 Disruption, Sham) and SRT<sub>EPOCH</sub> (SRT<sub>1</sub>, SRT<sub>2</sub>) as within-subject factors. The DT, the  
417 %Correct and the %TO data were analyzed using two-way ANOVA<sub>RM</sub> with SESSION (M1-  
418 Disruption, Sham) and TRIAL (obvious, ambiguous) as within-subject factors. The  
419 SumLogLR at DT was analyzed using a two-way ANOVA<sub>RM</sub> with SESSION (M1-  
420 Disruption, Sham) and BIN (Bin<sub>1</sub> to Bin<sub>7</sub>) as within-subject factors. When appropriate,  
421 Tukey's HSD post-hoc tests were used to detect paired differences in these ANOVAs.  
422 Furthermore, the intercept and the slope of the urgency functions were compared between the  
423 two sessions using Student's t-tests.

424

425 **RESULTS**

426 **Motor evoked potential data**

427 The ANOVA<sub>RM</sub> revealed a main effect of the factor SESSION on the percentage MEP  
428 amplitudes ( $F_{1,15} = 15.41$ ;  $p = .001$ ; see Figure 4). As such, percentage MEP amplitudes were  
429 lower following cTBS in the M1-Disruption session ( $78.78 \pm 3.04$  %) than in the Sham

430 session ( $105.53 \pm 5.32$  %; TMS<sub>1-7</sub> timings pooled together). The effect size (Cohen's *d*) for  
431 this factor was 1.5 indicating a large effect of SESSION (Cohen, 1988). This effect on  
432 percentage MEP amplitudes did not depend on time as the ANOVA<sub>RM</sub> did not reveal any  
433 effect of the factor TMS<sub>EPOCH</sub> ( $F_{6,90} = 1.99$ ,  $p = .075$ ) nor interaction with the factor SESSION  
434 ( $F_{6,90} = 0.72$ ,  $p = .637$ ). Hence, percentage MEP amplitudes remained stable following the  
435 cTBS intervention; they were consistently lower in the M1-Disruption than in the Sham  
436 session, regardless of the time at which MEPs were considered during the course of the  
437 experiment.

438 Additional single-sample Student's *t*-tests against 100 % (run for each TMS<sub>EPOCHS</sub>;  
439 Bonferroni-corrected at  $p < .0035$ ) showed that, as expected, the difference in MEP amplitude  
440 between the two sessions reported above was due to a selective suppression of MEPs in the  
441 M1-Disruption but not in the Sham session. As such, percentage MEP amplitudes were  
442 significantly lower than 100 % at almost all timings in the M1-Disruption session, except for  
443 TMS<sub>5</sub> and TMS<sub>7</sub> (*i.e.*, at TMS<sub>1-4</sub> and TMS<sub>6</sub>; all *p*-values = [.000008 .002]). Conversely,  
444 amplitudes were never significantly different from 100 % (*i.e.*, from TMS<sub>Baseline</sub>) in the Sham  
445 session (all *p*-values = [.163 .826]), indicating that right S1 cTBS had no impact on right M1  
446 activity, as previously reported (Derosiere et al., 2017a, 2017b).

447

## 448 **Behavioral data**

### 449 ***SRT Task***

450 The ANOVA<sub>RM</sub> revealed a main effect of the factor SESSION on the SRT data ( $F_{1,15} =$   
451  $5.34$ ,  $p = .035$ ; see Figure 5.A). Indeed, SRTs were significantly prolonged in the M1-  
452 Disruption session ( $237.3 \pm 7.4$  ms) compared to the Sham session ( $220.8 \pm 5.6$  ms; SRT<sub>1</sub> and  
453 SRT<sub>2</sub> pooled together). The effect size (Cohen's *d*) for this factor was 0.6 indicating a

454 medium to large effect of SESSION. The impact of M1 disruption on SRTs did not vary over  
455 the course of the session. As such, the ANOVA<sub>RM</sub> did not reveal any significant effect of the  
456 factor SRT<sub>EPOCH</sub> ( $F_{1,15} = 0.02$ ,  $p = .892$ ) nor of its interaction with the factor SESSION ( $F_{1,15} =$   
457  $1.78$ ,  $p = .202$ ). These findings indicated that M1-disruption altered the motor processes  
458 underlying initiation and/or execution of the cued movements (Huang et al., 2005; Lakhani et  
459 al., 2014; McAllister et al., 2013).

460

#### 461 *Tokens task*

##### 462 Decision time (DT)

463 As expected, the ANOVA<sub>RM</sub> revealed a main effect of the factor TRIAL on the DT data  
464 ( $F_{1,15} = 119.30$ ,  $p < .00001$ ; see Figure 5.B). Indeed, DTs were significantly shorter in obvious  
465 trials ( $871.77 \pm 57.14$  ms) than in ambiguous ones ( $1426.57 \pm 88.59$  ms; M1-Disruption and  
466 Sham sessions pooled together). Importantly, the ANOVA<sub>RM</sub> did not reveal any significant  
467 effect of the factor SESSION ( $F_{1,15} = 0.24$ ,  $p = .631$ ) nor of its interaction with the factor  
468 TRIAL ( $F_{1,15} = 0.02$ ,  $p = .888$ ). Hence, the time taken by the subjects to deliberate depended  
469 on the trial type they encountered (*i.e.*, obvious vs ambiguous) but was not affected by M1  
470 disruption.

471

##### 472 Percentage of correct choices (%Correct)

473 We found a significant main effect of the factor TRIAL for the %Correct data ( $F_{1,15} =$   
474  $31.727$ ,  $p = .00005$ ; see Figure 5.C). Indeed, %Correct was significantly higher in obvious  
475 trials ( $99.80 \pm 0.13$  %) than in ambiguous ones ( $88.61 \pm 1.80$  %; M1-Disruption and Sham  
476 sessions pooled together). However, neither the factor SESSION ( $F_{1,15} = 0.05$ ,  $p = .497$ ) nor

477 its interaction with the factor TRIAL were significant ( $F_{1,15} = 0.44$ ,  $p = .517$ ). Hence, M1  
478 disruption did not alter the accuracy of the decision process.

479

480

#### 481 Percentage of Time Out trials (%TO)

482 The %TO data revealed a similar pattern as the variables described above. Indeed, the  
483 %TO was significantly lower in obvious ( $0.20 \pm 0.13$  %) than in ambiguous trials ( $4.43 \pm 1.42$   
484 %; M1-Disruption and Sham sessions pooled together), as confirmed by the ANOVA<sub>RM</sub>  
485 (factor TRIAL:  $F_{1,15} = 7.47$ ,  $p = .015$ ; see Figure 5.D). Moreover, there was no effect of the  
486 factor SESSION ( $F_{1,15} = 0.01$ ,  $p = .920$ ) or interaction with the factor TRIAL ( $F_{1,15} = 0.01$ ,  $p =$   
487  $.922$ ). Hence, the proportion of trials in which subjects refrained from responding was  
488 unaffected by M1-Disruption.

489

#### 490 Sensory evidence at decision time (SumLogLR at DT) and urgency

491 The amount of sensory evidence based on which subjects made their decision was  
492 estimated using the SumLogLR (computed at DT): the higher the SumlogLR, the higher the  
493 evidence at DT (Cisek, 2009; Thura et al., 2012, 2014). SumLogLR values are presented for  
494 each Bin<sub>n</sub> on Figure 5.E (see *Methods*), separately for the M1-Disruption and the Sham  
495 sessions. Note that two subjects were excluded from this analysis as they responded too early  
496 on most trials, resulting in a lack of SumLogLR values after Jump<sub>9</sub> in these participants.  
497 Hence, SumLogLR analyses were run on 14 subjects.

498 Overall, fast decisions were made based on more sensory evidence than slow decisions,  
499 as confirmed by the ANOVA<sub>RM</sub> showing a main effect of the factor BIN on the SumLogLR at  
500 DT ( $F_{6,78} = 12.86$ ,  $p < .00001$ ; see Figure 5.E; BF value above 100). Indeed, Tukey HSD post-  
501 hoc tests showed that the SumLogLR at DT was significantly higher at Bin<sub>1</sub> ( $1.18 \pm 0.06$  a.u.)

502 than for any other bin after Bin<sub>4</sub> (all SumLogLR at DT  $\leq 0.84 \pm 0.05$  a.u.; M1-Disruption and  
503 Sham sessions pooled together). Hence, the amount of sensory evidence based on which  
504 subjects made their choices decreased as a function of time. Here again, the ANOVA<sub>RM</sub> did  
505 not reveal any significant effect of the factor SESSION ( $F_{6,78} = 0.04$ ,  $p = .852$ ) nor of its  
506 interaction with the factor BIN ( $F_{6,78} = 0.41$ ,  $p = .868$ ). Hence, subjects made their decisions  
507 based on a similar amount of sensory evidence in both sessions, suggesting a preservation of  
508 the urgency drive during deliberation with M1 disruption.

509 To further confirm this finding, we obtained a simple approximation of the urgency  
510 signal underlying the subjects' decisions by fitting a linear regression over the rectified  
511 version of SumLogLR at DT for each session (M1-Disruption, Sham) and extracted the  
512 intercept and the slope of the regression functions (see section *Methods* and Figure 5. F, G  
513 and H). Again, student t-tests did not reveal any significant impact of the session on the  
514 intercept ( $t_{14} = 0.48$ ,  $p = .798$ ) or the slope ( $t_{14} = -0.22$ ,  $p = .832$ ) of the urgency functions.

515

#### 516 Verifying that M1 disruption does not impact deliberation using Bayesian analyses

517 The ANOVA<sub>RM</sub> and the t-tests revealed that M1 disruption did not significantly alter the  
518 behavioral data measured in the tokens task, suggesting that M1 is not functionally involved  
519 in the deliberation process underlying action choices. In order to confirm this result, a Bayes  
520 Factor (BF) was computed for each analysis involving the factor SESSION (10 BF values  
521 obtained in total), providing us with a ratio of the likelihood probability of the null hypothesis  
522 (*i.e.*, H<sub>0</sub>: the probability that data do not exhibit an effect of SESSION) over the alternative  
523 hypothesis (*i.e.*, H<sub>1</sub>: the probability that data exhibit the effect; Morey and Rouder 2011). A  
524 BF value of 1 would reflect an equal probability that H<sub>0</sub> and H<sub>1</sub> are correct, while a BF value  
525 above 1 would reflect a higher probability that H<sub>0</sub> is correct. In accordance with conventional

526 interpretation of BF values (Jeffreys, 1961), a BF value ranging between 1 and 3 is interpreted  
 527 as indicating *anecdotal* evidence in favor of H0, a value between 3 and 10 as indicating  
 528 *substantial* evidence for H0 and a value between 10 and 30 a *strong* evidence for H0.

529 Table 1 summarizes the BF values obtained for each factor tested. The average BF value  
 530 was of  $5.66 \pm 1.74$  (all BFs ranged between 3.46 and 21.28) indicating substantial to strong  
 531 evidence for an absence of difference in subjects' behavior between the M1-Disruption and  
 532 the Sham sessions. Hence, Bayesian analyses further reinforce the conclusion that M1  
 533 disruption did not influence the deliberation process underlying decision-making, but solely  
 534 altered the motor processes that ensue commitment to an action.

535

Factor tested	DT	%Correct	%TO	SumLogLR	Urgency Intercept	Urgency Slope
SESSION	3.87	3.77	3.91	5.23	3.46	3.48
SESSION*TRIAL	3.91	3.77	3.91	---	---	---
SESSION*TIME	---	---	---	21.28	---	---

536

537 Table 1: Bayes factor (BF) values. The first column specifies the factors tested for which a BF  
 538 was computed. Other columns represent the BFs obtained for each behavioral measure in the  
 539 tokens task. Overall, BFs ranged between 3.46 and 21.28 indicating substantial to strong  
 540 evidence for a lack of effect of the SESSION on subjects' behavior.

541

## 542 DISCUSSION

543 Previous studies have shown that neural activity in motor cortical areas, including M1, is  
 544 strongly altered during decisions between actions (Alamia et al., 2018; Derosiere et al., 2018;  
 545 Donner et al., 2009; Gould et al., 2012; Klein-Flügge et al., 2012; Murphy et al., 2016;

546 Steinemann et al., 2018, Thura and Cisek, 2014a, 2016; Tosoni et al., 2008, 2014; Wyart et  
547 al., 2012). To date, however, the specific contribution of motor cortical areas to the decision  
548 process remains debated. Here, we asked whether M1 causally influences deliberation during  
549 action choices, or whether this area mostly contributes to the motor processes overtly  
550 expressing commitment. To do so, we tested the impact of a disruption of M1 activity,  
551 induced by continuous theta burst stimulation (cTBS), on the behavior of human subjects in  
552 (1) a simple reaction time (SRT) task allowing us to estimate the duration of the motor  
553 processes and (2) a modified version of the tokens task (Cisek et al., 2009), which allowed us  
554 to estimate subjects' time of commitment as well as their accuracy criterion.

555 Subjects were generally faster and more accurate in obvious than in ambiguous trials,  
556 suggesting that late decisions relied on weaker sensory evidence compared to early decisions.  
557 This is confirmed by the systematic analysis of the sensory evidence available at DT, which  
558 indicates that subjects committed to a choice based on less sensory evidence as time elapsed  
559 during the course of a trial. This dropping of the accuracy criterion is consistent with previous  
560 studies in which similar tasks were used (*e.g.*, Cisek et al., 2009; Gluth et al., 2012; Murphy et  
561 al., 2016; Thura et al., 2012, 2014;) and supports recent models postulating that urgency  
562 grows over time during speeded decisions (Churchland et al., 2008; Ditterich, 2006;  
563 Drugowitsch et al., 2012; Hanks et al., 2011).

564 The cTBS intervention reduced MEP amplitudes during the entire M1 disruption session,  
565 but never following a sham stimulation. Moreover, M1 cTBS lengthened the SRTs (*i.e.*,  
566 compared to when sham cTBS was performed), indicating that motor processes that are  
567 known to involve M1 were successfully perturbed by the intervention (Huang et al., 2005;  
568 Lakhani et al., 2014; McAllister et al., 2013). Notably, in the present study, motor responses  
569 were recorded through key-presses. Hence, RTs involved two periods, occurring before and  
570 after movement initiation (Spieser et al., 2017). As a consequence, it is sensible to assume that



571 the lengthening of SRT observed here might reflect an increase of (1) the time needed for  
572 initiating the required motor response, (2) the duration of the execution, or (3) both.

573 Critically, all the behavioral data collected in the tokens task were similar in the two  
574 cTBS sessions, whether M1 was disrupted or not. Based on this finding, the contribution of  
575 M1 to decision-making could be negligible. Hence, past reports of decision-related changes in  
576 M1 may reflect the influence of signals coming from upstream structures rather than an actual  
577 involvement in the deliberation process itself (Thura and Cisek, 2017; van Maanen et al.,  
578 2016). In a similar vein, our recent work shows that M1 disruption negatively alters value-  
579 based choices, but only when action values are freshly acquired. Such an effect of M1  
580 disruption does not occur anymore following consolidation. This suggests that M1  
581 contribution to value-based decision-making may vanish as subjects become more proficient  
582 at using the value information (Derosiere et al., 2015c; 2017a, 2017b). Thus, in well-learned  
583 decision-making tasks, the causal involvement of M1 might be restricted to the motor  
584 processes that follow commitment to an action.

585 However, there are alternative explanations for the lack of effect of M1 disruption on  
586 decision behavior in the present study. First, the behavioral variables extracted from the  
587 tokens task (*e.g.*, DT, decision accuracy, sensory evidence at DT, *etc.*) may not be sensitive  
588 enough to reflect the changes in decision behavior following disruption of motor cortical  
589 activity, contrary to the reaction times obtained in the SRT task. In line with this alternative  
590 interpretation, the absence of effect of M1 disruption in the tokens task would be due to a lack  
591 of sensitivity of the behavioral variables obtained in this specific task. Yet, the results of  
592 another study applying microstimulation in the premotor and motor cortex of non-human  
593 primates succeeded in altering decision behavior using the same task (Thura and Cisek,  
594 2014b). Hence, this suggests that the behavioral variables extracted from the tokens task are  
595 sensitive to the disruption of motor cortical activity.

596 Also, we cannot rule out the possibility that the cTBS intervention led to some fast  
597 reorganization of the decision network following M1 disruption. According to this idea, M1  
598 might still be part of the network involved in the deliberation process but some compensatory  
599 mechanisms may have occurred in this network following M1 disruption, leading to similar  
600 decision behaviors after M1 and sham cTBS (Bestmann et al., 2004; Briend et al., 2017; Cash  
601 et al., 2017; Derosiere et al., 2017a; Rastogi et al., 2017). One way to tackle this issue in the  
602 future would be to exploit online rTMS techniques (Duque et al., 2010, 2013), which allow  
603 one to perturb neural activity at a specific moment during the decision process, leaving less  
604 time for compensatory mechanisms to occur. As such, previous work has shown that while  
605 online microstimulation of a decision-related area alters behavior during perceptual decision-  
606 making (*i.e.*, the lateral intraparietal area; Hanks et al., 2006), (offline) inactivation of the  
607 same area does not (Katz et al., 2016).

608 Now, if the role of M1 is truly negligible, where in the brain are decisions about actions  
609 determined? Among many possible areas, PMd emerges as a promising candidate. First,  
610 single-cell recordings in behaving monkeys (Thura and Cisek, 2014a) have shown that during  
611 deliberation, activity of some PMd neurons tuned for a particular action reflects the unfolding  
612 sensory evidence favoring that action. This observation also makes it possible that this  
613 decision-related activity influences M1 neurons through cortico-cortical projections (Duque et  
614 al., 2012; Martinez-Gracia et al., 2015). Second, the same studies found that PMd activity  
615 related to the selected target reaches a peak about 280 ms before movement initiation  
616 regardless of decision difficulty, while a peak of M1 activity occurs about 140 ms later. Third,  
617 neurons in the globus pallidus internus, which are insensitive to sensory information during  
618 deliberation, become directionally tuned around the time of the PMd activity peak (Thura and  
619 Cisek, 2017). Altogether, these results suggest that PMd might be one of the primary sites  
620 where decision commitment is determined.

621 In agreement with this hypothesis, and as mentioned above, a recent study found that  
622 microstimulation of PMd neurons alters the deliberation duration, especially if current is  
623 applied shortly before commitment time (Thura and Cisek, 2014b). Crucially, stimulation has  
624 much less influence on decision duration if it is applied long before commitment or between  
625 commitment and movement onset. Relevant for the present work, this study also shows  
626 similar time-dependent effect of M1 microstimulation on decision durations – but the effect  
627 size is much smaller when M1 is stimulated compared to PMd. Finally, other non-primary  
628 motor areas may be causally involved in the deliberation process, including the pre-  
629 supplementary motor area (pre-SMA; Tosun et al., 2017). Investigating their precise  
630 contribution represents an interesting issue for future investigations.

631 In conclusion, we show that the offline disruption of M1 activity delays motor processes  
632 that follow commitment to an action, but does not alter volitional decision behavior. Taken  
633 together, these findings suggest that the contribution of M1 might be downstream of the  
634 decision process. Future studies should use online disruption protocols to deal with the  
635 putative network reorganization that may have occurred following offline M1 disruption in  
636 the present study and broaden their investigation to the role of non-primary motor areas in  
637 deliberation, especially the PMd and the pre-SMA.

638

## 639 REFERENCES

640 **Alamia A, Zénon A, VanRullen R, Duque J, Derosiere G.** Implicit visual cues tune  
641 oscillatory motor activity during decision-making. *Neuroimage* 186: 424–436, 2019.

642 **Alexandre F, Derosiere G, Pappiordanidou M, Billot M, Varray A.** Cortical motor output  
643 decreases after neuromuscular fatigue induced by electrical stimulation of the plantar flexor  
644 muscles. *Acta Physiol* 214: 124–134, 2015.

645 **Bestmann S, Baudewig J, Siebner HR, Rothwell JC, Frahm J.** Functional MRI of the  
646 immediate impact of transcranial magnetic stimulation on cortical and subcortical motor  
647 circuits. *Eur J Neurosci* 19: 1950–1962, 2004.

- 648 **Briend F, Leroux E, Delcroix N, Razafimandimby A, Etard O, Dollfus S.** Impact of rTMS  
649 on functional connectivity within the language network in schizophrenia patients with  
650 auditory hallucinations. *Schizophr Res* 189: 142–145, 2017.
- 651 **Cisek P, Puskas GA, El-Murr S.** Decisions in changing conditions: the urgency-gating  
652 model. *J Neurosci* 29: 11560–71, 2009.
- 653 **Clerget E, Andres M, Olivier E.** Deficit in Complex Sequence Processing after a Virtual  
654 Lesion of Left BA45. *PLoS One* 8: e63722, 2013.
- 655 **Cohen, J.** *Statistical Power Analysis for the Behavioral Sciences* (2nd ed.). Hillsdale, NJ  
656 Lawrence Erlbaum Associates, Publishers. 1988.
- 657 **Derosière G, Alexandre F, Bourdillon N, Mandrick K, Ward TE, Perrey S.** Similar  
658 scaling of contralateral and ipsilateral cortical responses during graded unimanual force  
659 generation. *Neuroimage* 85: 471–477, 2014.
- 660 **Derosiere G, Farrugia N, Perrey S, Ward T, Torre K.** Expectations induced by natural-like  
661 temporal fluctuations are independent of attention decrement: evidence from behavior and  
662 early visual evoked potentials. *Neuroimage* 104: 278–86, 2015a.
- 663 **Derosiere G, Zénon A, Alamia A, Klein PA, Duque J.** Contribution of primary motor  
664 cortex to perceptual and value-based decision processes. *Front Neurosci* 9, 2015b.
- 665 **Derosiere G, Klein P-A, Nozaradan S, Zénon A, Mouraux A, Duque J.** Visuomotor  
666 Correlates of Conflict Expectation in the Context of Motor Decisions. *J Neurosci* 38: 9486–  
667 9504, 2018.
- 668 **Derosiere G, Vassiliadis P, Demaret S, Zénon A, Duque J.** Learning stage-dependent effect  
669 of M1 disruption on value-based motor decisions. *Neuroimage* 162: 173–185, 2017a.
- 670 **Derosiere G, Zénon A, Alamia A, Duque J.** Primary motor cortex contributes to the  
671 implementation of implicit value-based rules during motor decisions. *Neuroimage* 146: 1115–  
672 1127, 2017b.
- 673 **Ditterich J.** Stochastic models of decisions about motion direction: Behavior and physiology.  
674 *Neural Network*. 19: 981–1012, 2006.
- 675 **Do M, Kirkovski M, Davies CB, Bekkali S, Byrne LK, Enticott PG.** Intra- and Inter-  
676 Regional Priming of Ipsilateral Human Primary Motor Cortex With Continuous Theta Burst  
677 Stimulation Does Not Induce Consistent Neuroplastic Effects. *Front Hum Neurosci* 12: 123,  
678 2018.
- 679 **Donner TH, Siegel M, Fries P, Engel AK.** Buildup of Choice-Predictive Activity in Human  
680 Motor Cortex during Perceptual Decision Making. *Curr Biol* 19: 1581–1585, 2009.
- 681 **Drugowitsch J, Moreno-Bote R, Churchland AK, Shadlen MN, Pouget A.** The Cost of  
682 Accumulating Evidence in Perceptual Decision Making. *J Neurosci*, 32:3612–3628. 2012.
- 683 **Duque J, Labruna L, Cazares C, Ivry RB.** Dissociating the influence of response selection  
684 and task anticipation on corticospinal suppression during response preparation.  
685 *Neuropsychologia* 65: 287–296, 2014.

- 686 **Duque J, Labruna L, Verset S, Olivier E, Ivry RB.** Dissociating the role of prefrontal and  
687 premotor cortices in controlling inhibitory mechanisms during motor preparation. *J Neurosci*  
688 32: 806–16, 2012.
- 689 **Duque J, Lew D, Mazzocchio R, Olivier E, Ivry RB.** Evidence for two concurrent  
690 inhibitory mechanisms during response preparation. *J Neurosci* 30: 3793–802, 2010.
- 691 **Duque J, Olivier E, Rushworth M.** Top–Down Inhibitory Control Exerted by the Medial  
692 Frontal Cortex during Action Selection under Conflict. *J Cogn Neurosci* 25: 1634–1648,  
693 2013.
- 694 **Economo MN, Viswanathan S, Tasic B, Bas E, Winnubst J, Menon V, Graybiuck LT,**  
695 **Nguyen TN, Smith KA, Yao Z, Wang L, Gerfen CR, Chandrashekar J, Zeng H, Looger**  
696 **LL, Svoboda K.** Distinct descending motor cortex pathways and their roles in movement.  
697 *Nature* 563: 79–84, 2018.
- 698 **Forstmann BU, Dutilh G, Brown S, Neumann J, von Cramon DY, Ridderinkhof KR,**  
699 **Wagenmakers E-J.** Striatum and pre-SMA facilitate decision-making under time pressure.  
700 *Proc Natl Acad Sci* 105: 17538–17542, 2008.
- 701 **Gluth S, Rieskamp J, Büchel C.** Deciding not to decide: computational and neural evidence  
702 for hidden behavior in sequential choice. *PLoS comp biol* 9:e1003309, 2012.
- 703 **Gould IC, Nobre AC, Wyart V, Rushworth MFS.** Effects of Decision Variables and  
704 Intraparietal Stimulation on Sensorimotor Oscillatory Activity in the Human Brain. *J*  
705 *Neurosci* 32: 13805–13818, 2012.
- 706 **Grandjean J, Derosiere G, Vassiliadis P, De Wilde Y, Quemener L, Duque J.** Towards  
707 assessing corticospinal excitability bilaterally: Validation of a double-coil TMS method. *J*  
708 *Neurosci Methods* 293: 162–168, 2018.
- 709 **Grent-'t-Jong T, Oostenveld R, Jensen O, Medendorp WP, Praamstra P.** Oscillatory  
710 dynamics of response competition in human sensorimotor cortex. *Neuroimage* 83: 27–34,  
711 2013.
- 712 **Hanks TD, Ditterich J, Shadlen MN.** Microstimulation of macaque area LIP affects  
713 decision-making in a motion discrimination task. *Nat Neurosci* 9: 682–689, 2006.
- 714 **Hanks TD, Mazurek ME, Kiani R, Hopp E, Shadlen MN.** Elapsed Decision Time Affects  
715 the Weighting of Prior Probability in a Perceptual Decision Task. *J Neurosci* 31:6339–6352,  
716 2011.
- 717 **Hauser TU, Moutoussis M, Purg N, Dayan P, Dolan RJ.** Beta-Blocker Propranolol  
718 Modulates Decision Urgency During Sequential Information Gathering. *J Neurosci* 38: 7170–  
719 7178, 2018.
- 720 **Herz DM, Tan H, Brittain JS, Fischer P, Cheeran B, Green AL, ... Foltynie T.** Distinct  
721 mechanisms mediate speed-accuracy adjustments in cortico-subthalamic networks. *Elife*, 6,  
722 e21481, 2017.
- 723 **Huang Y-Z, Edwards MJ, Rounis E, Bhatia KP, Rothwell JC.** Theta Burst Stimulation of  
724 the Human Motor Cortex. *Neuron* 45: 201–206, 2005.

725 **Jannati A, Block G, Oberman LM, Rotenberg A, Pascual-Leone A.** Interindividual  
726 variability in response to continuous theta-burst stimulation in healthy adults. *Clin*  
727 *Neurophysiol* 128: 2268–2278, 2017.

728 **Jeffreys H.** Theory of probability. Clarendon Press.  
729 [https://global.oup.com/academic/product/the-theory-of-probability-](https://global.oup.com/academic/product/the-theory-of-probability-9780198503682?cc=be&lang=en)  
730 [9780198503682?cc=be&lang=en](https://global.oup.com/academic/product/the-theory-of-probability-9780198503682?cc=be&lang=en) [6 Dec. 2018].

731 **Katz LN, Yates JL, Pillow JW, Huk AC.** Dissociated functional significance of decision-  
732 related activity in the primate dorsal stream. *Nature* 535: 285–288, 2016.

733 **Klein P-A, Olivier E, Duque J.** Influence of reward on corticospinal excitability during  
734 movement preparation. *J Neurosci* 32: 18124–36, 2012.

735 **Klein PA, Petitjean C, Olivier E, Duque J.** Top-down suppression of incompatible motor  
736 activations during response selection under conflict. *Neuroimage* 86: 138–149, 2014.

737 **Klein-Flügge MC, Bestmann S.** Time-dependent changes in human corticospinal excitability  
738 reveal value-based competition for action during decision processing. *J Neurosci* 32: 8373–  
739 82, 2012.

740 **Labruna L, Lebon F, Duque J, Klein P-A, Cazaes C, Ivry RB.** Generic inhibition of the  
741 selected movement and constrained inhibition of nonselected movements during response  
742 preparation. *J Cogn Neurosci* 26: 269–78, 2014.

743 **Lakhani B, Bolton DAE, Miyasike-daSilva V, Vette AH, McIlroy WE.** Speed of  
744 processing in the primary motor cortex: A continuous theta burst stimulation study. *Behav*  
745 *Brain Res* 261: 177–184, 2014.

746 **Laming DRJ.** Information theory of choice reaction time. Wiley; New York: 1968.

747 **Martinez-Garcia M, Insabato A, Pannunzi M, Pardo-Vazquez JL, Acuña C, Deco G.**  
748 The Encoding of Decision Difficulty and Movement Time in the Primate Premotor Cortex.  
749 *PLOS Comput Biol* 11: e1004502, 2015.

750 **Mcallister CJ, Rönnqvist KC, Stanford IM, Woodhall GL, Furlong PL, Hall SD.**  
751 Oscillatory Beta Activity Mediates Neuroplastic Effects of Motor Cortex Stimulation in  
752 Humans. *J Neurosci* 33: 7919-7927, 2013.

753 **Michelet T, Duncan GH, Cisek P.** Response Competition in the Primary Motor Cortex:  
754 Corticospinal Excitability Reflects Response Replacement During Simple Decisions. *J*  
755 *Neurophysiol* 104: 119–127, 2010.

756 **Morey RD, Rouder JN.** Bayes factor approaches for testing interval null hypotheses. *Psychol*  
757 *Methods* 16: 406–419, 2011.

758 **Murphy PR, Boonstra E, Nieuwenhuis S.** Global gain modulation generates time-dependent  
759 urgency during perceptual choice in humans. *Nat Commun* 7: 13526, 2016.

760 **Oberman L, Edwards D, Eldaief M, Pascual-Leone A.** Safety of Theta Burst Transcranial  
761 Magnetic Stimulation: A Systematic Review of the Literature. *J Clin Neurophysiol* 28: 67–74,  
762 2011.

- 763 **Pezzulo G, Cisek P.** Navigating the Affordance Landscape: Feedback Control as a Process  
764 Model of Behavior and Cognition. *Trends Cogn Sci* 20: 414–424, 2016.
- 765 **Quoilin C, Lambert J, Jacob B, Klein P-A, Duque J.** Comparison of Motor Inhibition in  
766 Variants of the Instructed-Delay Choice Reaction Time Task. *PLoS One* 11: e0161964, 2016.
- 767 **Quoilin C, Wilhelm E, Maurage P, de Timary P, Duque J.** Deficient inhibition in alcohol-  
768 dependence: let's consider the role of the motor system! *Neuropsychopharm*, 2018.
- 769 **Rastogi A, Cash R, Dunlop K, Vesia M, Kucyi A, Ghahremani A, Downar J, Chen J,**  
770 **Chen R.** Modulation of cognitive cerebello-cerebral functional connectivity by lateral  
771 cerebellar continuous theta burst stimulation. *Neuroimage* 158: 48–57, 2017.
- 772 **Ratcliff R.** A theory of memory retrieval. *Psych rev* 85:59, 1978.
- 773 **Reppert TR, Servant M, Heitz RP, Schall JD.** Neural mechanisms of speed-accuracy  
774 tradeoff of visual search: saccade vigor, the origin of targeting errors, and comparison of the  
775 superior colliculus and frontal eye field. *J Neurophysiol* 120: 372–384, 2018.
- 776 **Rocchi L, Ibáñez J, Benussi A, Hannah R, Rawji V, Casula E, Rothwell J.** Variability and  
777 Predictors of Response to Continuous Theta Burst Stimulation: A TMS-EEG Study. *Front*  
778 *Neurosci* 12: 400, 2018.
- 779 **Rossini PM, Barker AT, Berardelli A, Caramia MD, Caruso G, Cracco RQ, Dimitrijević**  
780 **MR, Hallett M, Katayama Y, Lücking CH, Maertens de Noordhout AL, Marsden CD,**  
781 **Murray NMF, Rothwell JC, Swash M, Tomberg C.** Non-invasive electrical and magnetic  
782 stimulation of the brain, spinal cord and roots: basic principles and procedures for routine  
783 clinical application. Report of an IFCN committee. *Electroencephalogr Clin Neurophysiol* 91:  
784 79–92, 1994.
- 785 **Rossini PM, Burke D, Chen R, Cohen LG, Daskalakis Z, Di Iorio R, Di Lazzaro V,**  
786 **Ferreri F, Fitzgerald PB, George MS, Hallett M, Lefaucheur JP, Langguth B,**  
787 **Matsumoto H, Miniussi C, Nitsche MA, Pascual-Leone A, Paulus W, Rossi S, Rothwell**  
788 **JC, Siebner HR, Ugawa Y, Walsh V, Ziemann U.** Non-invasive electrical and magnetic  
789 stimulation of the brain, spinal cord, roots and peripheral nerves: Basic principles and  
790 procedures for routine clinical and research application. An updated report from an I.F.C.N.  
791 Committee. *Clin Neurophysiol* 126: 1071–1107, 2015.
- 792 **Rothwell JC, Thompson PD, Day BL, Boyd S, Marsden CD.** Stimulation of the human  
793 motor cortex through the scalp. [Online]. *Exp Physiol* 76: 159–200, 1991.  
794 <http://www.ncbi.nlm.nih.gov/pubmed/2059424> [12 Mar. 2019].
- 795 **Sasaki T, Kodama S, Togashi N, Shirota Y, Sugiyama Y, Tokushige S, Inomata-Terada**  
796 **S, Terao Y, Ugawa Y, Hamada M.** The intensity of continuous theta burst stimulation, but  
797 not the waveform used to elicit motor evoked potentials, influences its outcome in the human  
798 motor cortex. *Brain Stimul* 11: 400–410, 2018.
- 799 **Schmidt C, Peigneux P, Muto V, Schenkel M, Knoblauch V, Münch M, de Quervain DJ-**  
800 **F, Wirz-Justice A, Cajochen C.** Encoding Difficulty Promotes Postlearning Changes in  
801 Sleep Spindle Activity during Napping. *J Neurosci* 26: 8976–8982, 2006.

- 802 **Seideman JA, Stanford TR, Salinas E.** Saccade metrics reflect decision-making dynamics  
803 during urgent choices. *Nat Commun* 9: 2907, 2018.
- 804 **Solopchuk O, Alamia A, Dricot L, Duque J, Zénon A.** cTBS disruption of the  
805 supplementary motor area perturbs cortical sequence representation but not behavioural  
806 performance. *Neuroimage* 163: 34–40, 2017.
- 807 **Spieser L, Servant M, Hasbroucq T, Burle B.** Beyond decision! Motor contribution to  
808 speed–accuracy trade-off in decision-making. *Psychon Bull Rev* 24: 950–956, 2017.
- 809 **Steinemann NA, O'Connell RG, Kelly SP.** Decisions are expedited through multiple neural  
810 adjustments spanning the sensorimotor hierarchy. *Nat. Commun* 9(1):3627, 2018.
- 811 **Stone M.** Models for choice-reaction time. *Psychometrika* 25:251-260, 1960.
- 812 **Summerside EM, Shadmehr R, Ahmed AA.** Vigor of reaching movements: reward  
813 discounts the cost of effort. *J Neurophysiol* 119: 2347–2357, 2018.
- 814 **Svoboda K, Li N.** Neural mechanisms of movement planning: motor cortex and beyond. *Curr*  
815 *Opin Neurobiol* 49: 33–41, 2018.
- 816 **Thura D, Beauregard-Racine J, Fradet C-W, Cisek P.** Decision making by urgency gating:  
817 theory and experimental support. *J Neurophysiol* 108: 2912–2930, 2012.
- 818 **Thura D, Cisek P.** Deliberation and Commitment in the Premotor and Primary Motor Cortex  
819 during Dynamic Decision Making. *Neuron* 81: 1401–1416, 2014a.
- 820 **Thura D, Cisek P.** Micro-stimulation of premotor and motor cortex delays the commitment  
821 to an action choice. Program No. 651.04. 2014 Neuroscience Meeting Planner. Washington,  
822 DC: Society for Neuroscience, 2014b.
- 823 **Thura D, Cisek P.** Modulation of premotor and primary motor cortical activity during  
824 volitional adjustments of speed-accuracy trade-offs. *J Neurosci* 36: 938-956. 2016
- 825 **Thura D, Cisek P.** The Basal Ganglia Do Not Select Reach Targets but Control the Urgency  
826 of Commitment. *Neuron* 95: 1160–1170.e5, 2017.
- 827 **Thura D, Cos I, Trung J, Cisek P.** Context-dependent urgency influences speed-accuracy  
828 trade-offs in decision-making and movement execution. *J Neurosci* 34: 16442–54, 2014.
- 829 **Torta D, Legrain V, Algoet M, Olivier E, Duque J, Mouraux A.** Theta Burst Stimulation  
830 Applied over Primary Motor and Somatosensory Cortices Produces Analgesia Unrelated to  
831 the Changes in Nociceptive Event-Related Potentials. *PloS One* 8: e73263, 2013.
- 832 **Tosoni A, Corbetta M, Calluso C, Committeri G, Pezzulo G, Romani GL, Galati G.**  
833 Decision and action planning signals in human posterior parietal cortex during delayed  
834 perceptual choices. *Eur J Neurosci* 39: 1370–1383, 2014.
- 835 **Tosun T, Berkay D, Sack AT, Çakmak YÖ, Balci F.** Inhibition of Pre-Supplementary  
836 Motor Area by Continuous Theta Burst Stimulation Leads to More Cautious Decision-making  
837 and More Efficient Sensory Evidence Integration. *J Cogn Neurosci* 29: 1433–1444, 2017.
- 838 **van Maanen L, Fontanesi L, Hawkins GE, Forstmann BU.** Striatal activation reflects  
839 urgency in perceptual decision making. *Neuroimage* 139: 294–303, 2016.



- 840 **Vandermeeren Y, Davare M, Duque J, Olivier E.** Reorganization of cortical hand  
841 representation in congenital hemiplegia. *Eur J Neurosci* 29: 845–854, 2009.
- 842 **Vassiliadis P, Grandjean J, Derosiere G, de Wilde Y, Quemener L, Duque J.** Using a  
843 Double-Coil TMS Protocol to Assess Preparatory Inhibition Bilaterally. *Front Neurosci* 12:  
844 139, 2018.
- 845 **Waldert S, Vigneswaran G, Philipp R, Lemon RN, Kraskov A.** Modulation of the  
846 Intracortical LFP during Action Execution and Observation. *J Neurosci* 35: 8451–61, 2015.
- 847 **Wyart V, de Gardelle V, Scholl J, Summerfield C.** Rhythmic Fluctuations in Evidence  
848 Accumulation during Decision Making in the Human Brain. *Neuron* 76: 847–858, 2012.
- 849 **Yoon T, Geary RB, Ahmed AA, Shadmehr R.** Control of movement vigor and decision  
850 making during foraging. *Proc Natl Acad Sci U S A* 115: E10476–E10485, 2018.
- 851 **Zénon A, Klein P-A, Alamia A, Boursoit F, Wilhelm E, Duque J.** Increased Reliance on  
852 Value-based Decision Processes Following Motor Cortex Disruption. *Brain Stimul* 8: 957–  
853 964, 2015.

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859

#### 860 **AUTHOR CONTRIBUTIONS**

861 G.D., D.T., P.C. and J.D. conceived and designed research; G.D. performed experiments;  
862 G.D. analyzed data; G.D., D.T., P.C. and J.D. interpreted results of experiments; G.D.  
863 prepared figures; G.D. and J.D. drafted manuscript; G.D., D.T., P.C. and J.D. edited and  
864 revised manuscript; G.D., D.T., P.C. and J.D. approved final version of manuscript.

865

#### 866 **DISCLOSURES**

867 No conflicts of interest, financial or otherwise, are declared by the authors.

868

#### 869 **FIGURE LEGENDS**

870 Fig.1. Schematic of the tokens task. In each trial, 15 tokens jumped one-by-one every 200 ms  
871 from the central circle to one of the two lateral circles (*i.e.*,  $\text{Jump}_1$  to  $\text{Jump}_{15}$ ). The subjects  
872 had to indicate by a right index or right middle finger key-press (*i.e.*, F9 and F8 keys,

873 respectively) which lateral circle they thought would receive more tokens (*i.e.*, left or right  
874 circle, respectively) at the end of the trial. They could provide their response whenever they  
875 wanted between Jump<sub>1</sub> and Jump<sub>15</sub>. For a correct response, the subjects earned, in € cents, the  
876 number of tokens remaining in the central circle at the time of the response. Hence, the  
877 reward received for a correct response decreased over time, as depicted on the upper right side  
878 of the figure (green trace). The example presented on the lower left side of the figure  
879 represents a correct response provided between Jump<sub>9</sub> and Jump<sub>10</sub> (*i.e.*, the score indicates  
880 that 6 tokens remained in the central circle at the moment the right circle was chosen). In  
881 contrast, if subjects chose the incorrect lateral circle, they lost 7 € cents, regardless of their  
882 RT. As such, the penalty score was fixed, as shown in red on the upper right side of the  
883 figure: the lower middle example represents an incorrect choice of the left circle. Thus, the  
884 reward/penalty ratio decreased over time, producing an increasing sense of urgency over the  
885 course of a trial. In the absence of response (“Time Out” trial, lower right side example),  
886 subjects were neither rewarded, nor penalized (score = 0). For representative purposes, the  
887 “Time Out” message is depicted below the circles in this example, while it was presented  
888 above them in the experiment.

889

890 Fig. 2. Experimental protocol. Subjects came to the lab for 3 consecutive days (Day 1, 2 and  
891 3). On each day, they performed the tokens task during 4 blocks of 50 trials (Block<sub>1-4</sub>; light  
892 gray rectangles). They also performed Simple Reaction Time blocks at the beginning and at  
893 the end of each session (SRT<sub>1</sub> and SRT<sub>2</sub>, respectively; dark gray rectangles). Day 1 served as  
894 a training session and did not involve any continuous Theta Burst Stimulation (cTBS). A  
895 cTBS train was applied for 40 s at the beginning of Day 2 and 3 (red rectangles), either over  
896 the left (L) primary motor cortex (M1-Disruption session, black coil) or over the right (R)  
897 primary somatosensory cortex (Sham session, gray coil), in a randomized order. Motor  
898 Evoked Potentials (MEPs) were elicited at different time points (TMS<sub>EPOCHS</sub>) throughout the  
899 sessions (TMS<sub>Baseline</sub> and TMS<sub>1-7</sub>, yellow rectangles), either in the R first dorsal interosseous  
900 (FDI) muscle (M1-Disruption session) or in the L FDI (Sham session), by applying single-  
901 pulse TMS over the L or R M1, respectively. Note that in the Sham session, this implied  
902 targeting different sites for the cTBS intervention (R S1) and the MEP assessments (R M1;  
903 coil position not shown on the figure).

904

905 Fig.3. Urgency function estimation. We exploited the SumLogLR values to estimate the level  
906 of urgency at DT for each subject *i* and each session *j*. To do so, we followed four steps  
907 (shown from left to right). First, SumLogLR values were obtained for different bins of DT.  
908 Then, these values were multiplied by -1. Next, a constant of 3 was added to obtain positive  
909 values. Finally, a linear regression was fitted over the positive values. The equation of the  
910 regression allowed us to extract the intercept and the slope of the obtained urgency function  
911 (1.79 and 0.06 in this example, respectively).

912

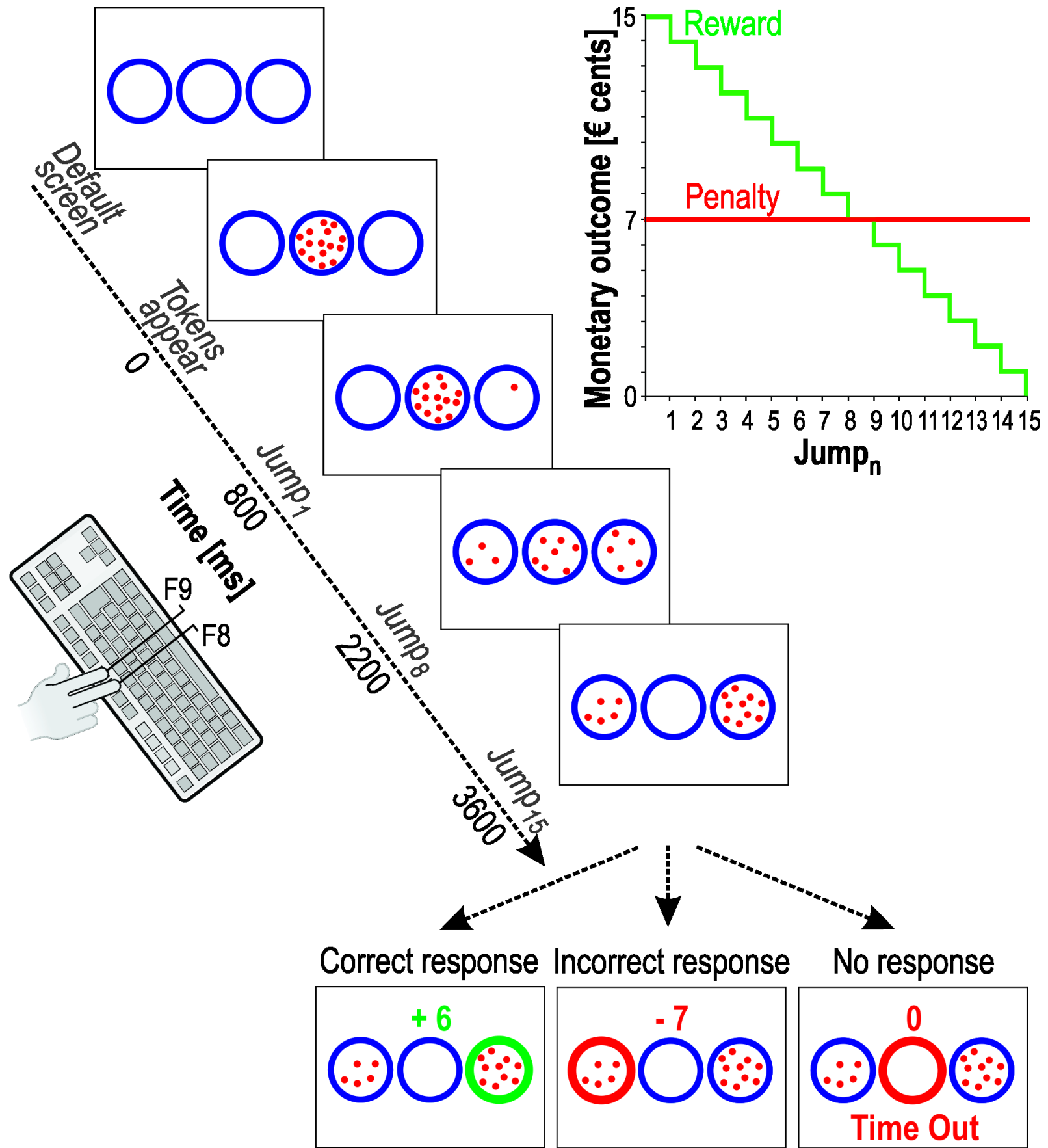
913 Fig. 4. Motor Evoked Potentials (MEPs) amplitudes. A. Mean value of MEPs (in percentage  
914 of MEPs at TMS<sub>Baseline</sub>) elicited after the cTBS intervention in the First Dorsal Interosseous  
915 (FDI) muscle at each of the TMS<sub>EPOCHS</sub> (TMS<sub>1-7</sub>) in the M1-Disruption (black traces) and  
916 Sham (gray traces) sessions. Note the significant disruption of MEPs with respect to baseline

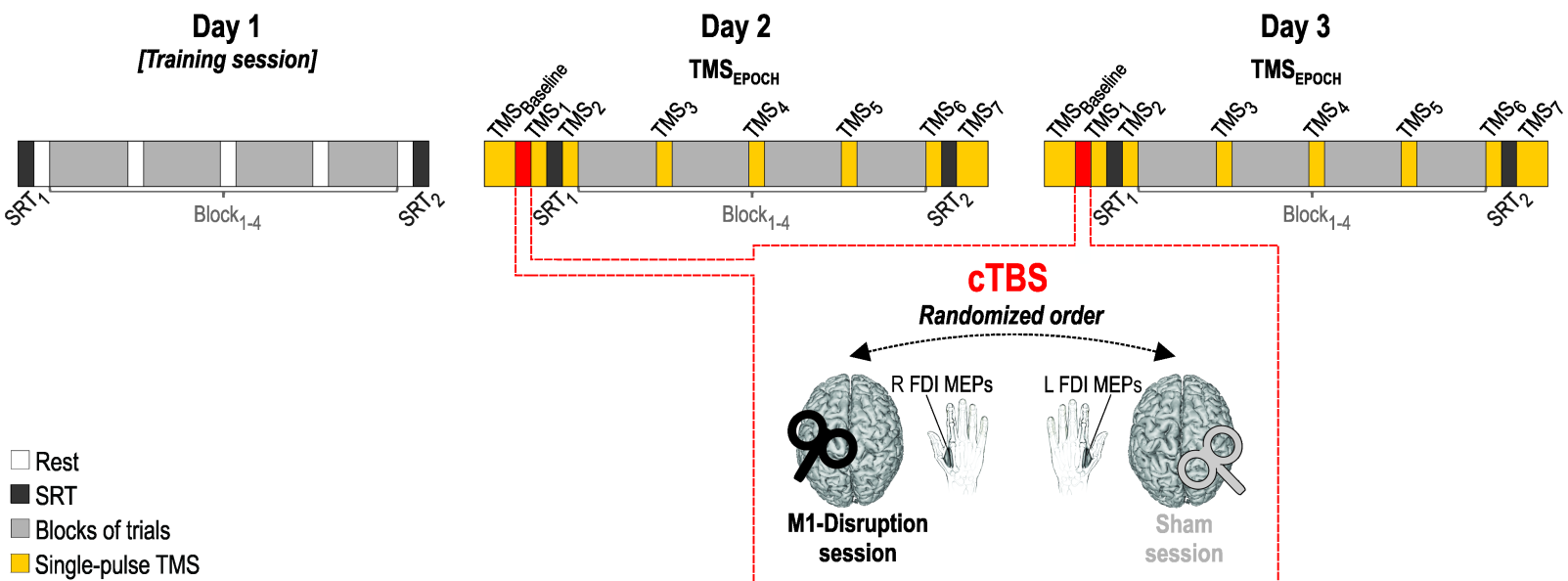
917 (*i.e.*, dashed horizontal line) in the M1-Disruption session (#: significantly different from 100  
918 at  $p < .0036$  [Bonferroni-corrected]; ¥: significantly different from 100 at  $p < .05$   
919 [uncorrected;  $p = .017$ ]). *B.* Cumulative percentage of subjects. MEPs obtained at TMS<sub>1-7</sub> are  
920 pooled together. Note that all subjects included in the analysis showed percentage MEP  
921 amplitudes smaller than 100% in the M1-disruption (*i.e.*, a disruptive effect), while the same  
922 subjects did not show any effect in the Sham session, as also shown in the inset representing  
923 the group-level average with the effect of SESSION (\*: significantly different at  $p < .05$ ).  
924 Error bars represent SE. *C.* Example of single-trial MEP recordings Each trace depicts a raw  
925 EMG signal in a representative subject (#18), starting 20 ms before the TMS pulse and ending  
926 100 ms after it. The artifact caused by the pulse is reflected as a peak occurring at time 0; the  
927 MEP occurs approximately 22 ms later. The four recordings display MEPs elicited at  
928 TMS<sub>Baseline</sub> (left) or TMS<sub>3</sub> (right) in the M1-Disruption (black traces) or Sham (gray traces)  
929 session. In this subject, cTBS had a strong effect; average percentage MEP amplitudes at  
930 TMS<sub>3</sub> were much smaller in the M1-Disruption session ( $66 \pm 12.8\%$ ) compared to the sham  
931 session ( $112.6 \pm 5.7\%$ ).

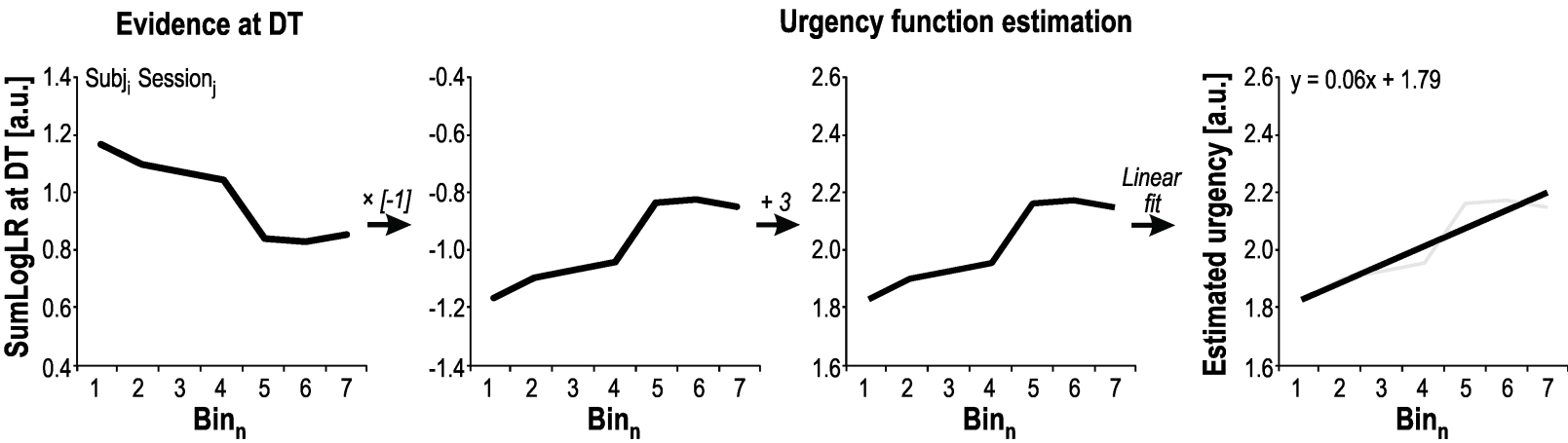
932

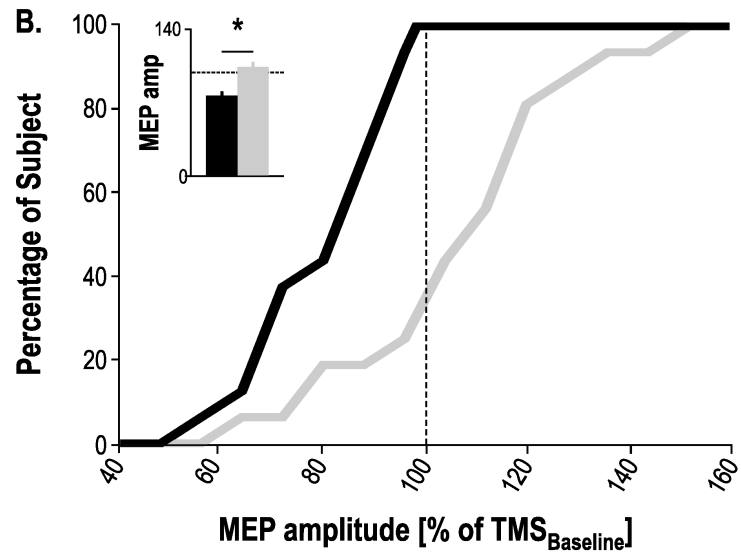
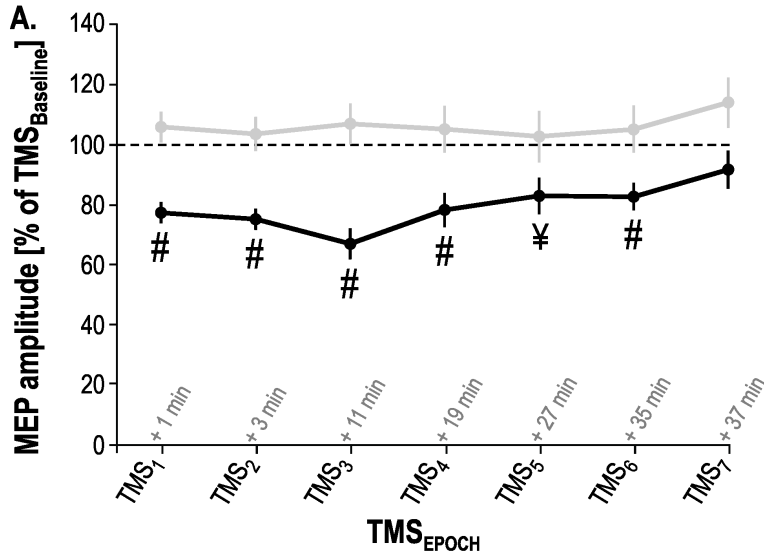
933 Fig. 5. Behavioral results. *A.* Mean Simple Reaction Time (SRT) (obtained in the SRT task)  
934 measured at each of the SRT<sub>EPOCHS</sub> (SRT<sub>1-2</sub>) in the M1-Disruption (black bars) and Sham  
935 (gray bars) sessions. *B.* Mean Decision Time (DT) measured in each TRIAL (obvious,  
936 ambiguous) in the M1-Disruption (black bars) and Sham (gray bars) sessions. *C* and *D* same  
937 as *B* for the percentages of correct choices (%Correct) and of Time Out trials (%TO),  
938 respectively. *E.* SumLogLR at DT measured in each Bin<sub>n</sub> of decision time (*i.e.*, between  
939 Jump<sub>5</sub> and Jump<sub>12</sub>, see main text) in the M1-Disruption (black traces) and Sham (gray traces)  
940 sessions. *F.* Urgency functions computed based on the rectified SumLogLR at DT for the M1-  
941 Disruption (black traces) and Sham (gray traces) sessions. The small bar graphs on the bottom  
942 right represent the group-level average intercept and slope of the functions. Light lines  
943 illustrate individual estimated urgency functions, bold lines illustrate the mean urgency  
944 functions averaged across population. *G.* Individual intercept values, represented for the M1-  
945 Disruption Session (y-axis) as a function of the values for the Sham session (x-axis). Points  
946 above the diagonal ( $n = 7/14$ ) represent the subjects showing a higher intercept in the M1-  
947 Disruption than following Sham session, while points below the diagonal ( $n = 7/14$ ) represent  
948 the subjects showing a lower intercept in the M1-Disruption than following Sham session. *H.*  
949 Same as *G.* for the slope values. \*: significant difference ( $p < .05$ ). Error bars represent SE.

950









**C.** Example of single-trial MEP recordings - Subject 18

