

1 Full title: Isoflurane and Ketamine Differentially Influence Spontaneous and Evoked Laminar  
2 Electrophysiology in Mouse V1

3 Abbreviated title: Laminar Electrophysiological Analysis of Isoflurane and Ketamine Anesthesia

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## 12 **Abstract**

13 General anesthesia is ubiquitous in research and medicine, yet although the molecular mechanisms of  
14 anesthetics are well characterized, their ultimate influence on cortical electrophysiology remains  
15 unclear. Moreover, the influence that different anesthetics have on sensory cortices at neuronal and  
16 ensemble scales is mostly unknown, and represents an important gap in knowledge that has widespread  
17 relevance for neural sciences. To address this knowledge gap, this work explored the effects of  
18 isoflurane and ketamine/xylazine, two widely used anesthetic paradigms, on electrophysiological  
19 behavior in mouse primary visual cortex. First, multiunit activity and local field potentials were  
20 examined to understand how each anesthetic influences spontaneous activity. Then, the inter-laminar  
21 relationships between populations of neurons at different cortical depths were studied to assess  
22 whether anesthetics influenced resting-state functional connectivity. Lastly, the spatiotemporal  
23 dynamics of visually evoked multiunit and local field potentials were examined to determine how each  
24 anesthetic alters communication of visual information. We found that isoflurane enhanced the

25 rhythmicity of spontaneous ensemble activity at 10-40 Hz, which coincided with large increases in  
26 coherence between layer IV with superficial and deep layers. Ketamine preferentially increased local  
27 field potential power from 2-4 Hz, and the largest increases in coherence were observed between  
28 superficial and deep layers. Visually evoked responses across layers were diminished under isoflurane,  
29 and enhanced under ketamine anesthesia. These findings demonstrate that isoflurane and ketamine  
30 anesthesia differentially impact sensory processing in V1.

31 **NEW & NOTEWORTHY** We directly compared electrophysiological responses in awake and anesthetized  
32 (isoflurane or ketamine) mice. We also propose a method for quantifying and visualizing highly variable,  
33 evoked multiunit activity. Lastly, we observed distinct oscillatory responses to stimulus onset and offset  
34 in awake and isoflurane anesthetized mice.

35 **Keywords:** anesthesia, laminar electrophysiology, spontaneous, evoked

## 36 INTRODUCTION

37 In 1846, the first successful surgery under general anesthesia was performed, thereafter  
38 revolutionizing the practice of medicine (Robinson and Toledo 2012). Yet after more than a century of  
39 clinical ubiquity, a detailed understanding of the micro and mesoscale mechanisms of anesthesia and  
40 anesthetic induced loss of consciousness remains elusive. Consciousness is thought to emerge from the  
41 integration of information generated from subsystems across the brain (Tononi 2008). Accordingly,  
42 anesthetic induced unconsciousness is characterized by disruption of communication between cortical  
43 or subcortical networks (Alkire et al. 2008; Franks 2008; Hudetz 2012; Mashour and Hudetz 2018). To  
44 this end, many studies have investigated how various anesthetics influence or restrict large-scale  
45 functional communication between brain regions (Boveroux et al. 2010; Cimenser et al. 2011; Schroeder  
46 et al. 2016; Sellers et al. 2015; Supp et al. 2011).

47 Fewer studies, however, explore the effects of anesthesia at the local ensemble scales. Yet  
48 growing evidence suggests that anesthetics have a profound influence on neuronal network activity

49 within cortical subsystems. For example, anesthetics have been shown to alter the balance between  
50 excitation and inhibition (Haider et al. 2013; Homayoun and Moghaddam 2007), modulate oscillatory  
51 ensemble activity (Chery et al. 2014; Hakami et al. 2009; Imas et al. 2004; Imas et al. 2005), and  
52 influence neuronal response properties (Duncan et al. 1982; Goltstein et al. 2015). These changes in  
53 neuronal activity are important to characterize since many seminal neuroscience studies have been  
54 conducted in anesthetized animals, and a detailed understanding of the electrophysiological effects of  
55 anesthetics may be critical for an accurate interpretation of results.

56 Moreover, numerous anesthetic agents, which have distinct molecular targets,  
57 electrophysiological features, and act with regional specificity, have been widely used throughout the  
58 literature (Brown et al. 2011; Cavazzuti et al. 1987). Direct comparisons of anesthetic classes have  
59 revealed substantial variability in altered electrophysiological behavior (Cederholm et al. 2012; Furmaga  
60 et al. 2014; Hayton et al. 1999; Ruebhausen et al. 2012; Sarasso et al. 2015; Woodward et al. 2007). A  
61 detailed comparison of micro and mesoscale cortical activity between anesthetic classes may therefore  
62 provide further insight into the mechanistic actions of anesthetics. The present work compares network  
63 activity using a linear electrode array, under isoflurane and ketamine/xylazine (KX) anesthesia, two  
64 commonly used anesthetic paradigms in neuroscience research.

65 Isoflurane is a volatile anesthetic, which acts primarily via potentiation of inhibitory GABA<sub>A</sub>  
66 (gamma-aminobutyric acid type A) receptors, but also through inhibition of glutamatergic AMPA ( $\alpha$ -  
67 amino-3-hydroxy-5-methyl-4-isoxazolepropionic acid) and NMDA (N-methyl-D-aspartate) receptors  
68 (Alkire et al. 2008; Dildy-Mayfield et al. 1996; Kimbro et al. 2000). Isoflurane administration affects  
69 cortical activity in a dose-dependent fashion, progressing towards burst suppression at high  
70 concentrations, which is characterized by quasi-periodic alternations of high amplitude bursting activity  
71 followed by prolonged periods of suppressed activity (Ferron et al. 2009). In sensory cortices, isoflurane  
72 augments spontaneous and evoked local field potential (LFP) oscillations (Imas et al. 2005; Sellers et al.

73 2013; Sellers et al. 2015), and alters the spatial and temporal dynamics of evoked multiunit activity  
74 (MUA), possibly as a result of diminished inhibition (Haider et al. 2013).

75 Ketamine, a dissociative anesthetic, acts primarily via inhibition of NMDA receptors, but also  
76 through minor potentiation of GABA<sub>A</sub> receptors (Alkire et al. 2008; Brown et al. 2011). It is often used  
77 with the sedative xylazine, an  $\alpha_2$  adrenergic receptor agonist. In cortex, ketamine produces disinhibited  
78 excitation, and strongly influences oscillatory LFP, particularly by inducing prominent slow wave activity  
79 (Chauvette et al. 2011; Fiáth et al. 2016; Steriade et al. 1993b) and modulating gamma frequencies  
80 (Anver et al. 2011; Caixeta et al. 2013; Chery et al. 2014; Hakami et al. 2009; Shaw et al. 2015).  
81 Interestingly, ketamine shares similar electrophysiological abnormalities with schizophrenia (Caixeta et  
82 al. 2013; Ehrlichman et al. 2009).

83 Although isoflurane and ketamine have been extensively studied independently, this study aims  
84 to build upon this body of knowledge by directly comparing laminar electrophysiological activity within  
85 the same animals. Recordings were collected from mouse V1 because the functional architecture of the  
86 visual system is well documented; information flows from layer IV to II/III, then V (Douglas and Martin  
87 2004; Hirsch and Martinez 2006). Additionally, recordings from the visual cortex provide the capability  
88 to examine spontaneous and evoked activity. To this end, we examined multiunit activity and local field  
89 potentials to provide insight into the functional changes in individual neurons, as well as the summated  
90 population activity within the surrounding area. Isoflurane and ketamine were found to produce  
91 spatiotemporally and rhythmically distinct patterns of spontaneous and evoked electrophysiological  
92 activity, suggesting that processing within V1 is differentially influenced by each anesthetic.

### 93 **METHODS**

94 All experimental protocols were approved by the University of Pittsburgh's Institutional Animal Care and  
95 Use Committee.

#### 96 *Surgical Procedure*

97 Surgical procedures were carried out as previously described (Kozai et al. 2015a; Kozai et al.  
98 2015b; Kozai et al. 2014; Michelson et al. 2017). 9-week old female C57BL/6 mice (22-28g) were placed  
99 in a stereotaxic frame (Kopf Instruments, Tujunga, CA) and induced with 1.5–2% isoflurane with oxygen  
100 flow at 1 L/min, and then maintained at 1.25–1.5%. Throughout the procedure, body temperature was  
101 maintained using a warm water pad (HTP 1500, Adroit Medical Systems, Loudon TN). After the skin and  
102 connective tissue over the skull were removed, a thin layer of Vetbond (3 M) was applied to the skull. A  
103 small craniotomy was made over visual cortex with a high-speed dental drill. The drilling procedure was  
104 periodically interrupted, and the surface of the skull rinsed with a saline solution to prevent damaging  
105 heat transfer to the brain. Three bone screws were placed into the skull, one over the contralateral  
106 visual cortex and two bilaterally over motor cortex.

107 A 16-channel, planar silicon Michigan electrode (single shank, 3mm long, recording sites spaced  
108 100µm apart; A1 × 16-3mm-100-703-CM16LP, Neuronexus Technologies, Ann Arbor, MI) was implanted  
109 into the left monocular visual cortex (1.0mm anterior to lambda, 1.5mm lateral from midline). The array  
110 was inserted at ~1mm/s to a depth of 1.6mm, using a hand-driven micromanipulator, such that the top  
111 edge of the top-most recording site was at the surface of the brain, and the recording sites faced away  
112 from the midline, toward V1m/V1b. The reference wire was connected to the ipsilateral bone screw  
113 over the motor cortex, and the preamplifier ground wire was shorted to the contralateral bone screws  
114 over the motor and visual cortex. After insertion, the craniotomy was filled, and the electrode was  
115 protected with Kwik-sil. The electrode and bone screws were then cemented into place with dental  
116 cement (Pentron Clinical, Orange, CA). After the procedure, 3cc of Ringer's solution was injected  
117 subcutaneously to the back of the animal to aid recovery. Buprenorphine (0.3 mg/kg) was administered  
118 twice daily for three days as a post-operative analgesic.

119 *Neurophysiological Recording*

120           Chronic electrophysiological recordings (183-190 days post-implant) were conducted from  
121 within a grounded, but otherwise electrically isolated faraday cage. Each animal was recorded for a  
122 single time-point. A 24" LCD screen (V243H, Acer. Xizhi, New Taipei City, Taiwan) was placed just outside  
123 of the cage for presentation of visual stimulus. Recorded data was transferred through a nonconductive  
124 optic fiber out of the cage, using a battery-powered preamplifier (Medusa preamp, Tucker-Davis  
125 Technologies, Alachua, FL), which was housed inside the cage (Kozai et al. 2012).

126           Animals were placed on a microwaveable heating pad (Deltaphase isothermal pad, Braintree  
127 Scientific, Inc, Braintree, MA) (1.6 mm mesh), with the head mechanically fixed using a custom-built  
128 stereotaxic frame. The animal was placed 20cm from the monitor on the side contralateral to the site of  
129 implantation, spanning a total visual field of 120° wide by 60° high. Recordings were conducted in a dark  
130 room and consisted of 130s epochs of spontaneous and visually evoked signals, sampled at 24kHz.  
131 Spontaneous recordings were taken with the monitor turned off. For the evoked recordings, visual  
132 stimuli were presented using the MATLAB-based Psychophysics Toolbox (Psychtoolbox) (Brainard 1997;  
133 Kleiner et al. 2007; Pelli 1997). Stimuli consisted of full-field solid black and white drifting gratings in  
134 vertical or 45° directions. Timing of the visual stimulus was synchronized to the recording system (RX5,  
135 Tucker-Davis Technologies, Alachua FL) via transistor-transistor logic (TTL) pulses sent from the display  
136 computer through a stimulus isolator (A-M Systems Model 2200). 64 visually evoked trials were  
137 conducted throughout the recording epoch, where each trial consisted of 1 second of stimulus  
138 presentation followed by a 1 second dark screen period (Cody et al. 2018; Kolarcik et al. 2015; Kozai et  
139 al. 2016; Kozai et al. 2015b), hereafter referred to as ON and OFF periods.

140           Six animals were examined in this study. Data were first collected from lightly isoflurane-  
141 anesthetized animals. Recordings began 10 minutes following isoflurane induction. Dosage was  
142 maintained at the lowest concentration sufficient for inducing animal inactivity while avoiding burst  
143 suppression (Kozai et al. 2015b) (~1.1%). Animals were carefully monitored during recording to ensure

144 that this level of anesthesia was maintained. Following data collection, isoflurane administration ceased,  
145 and animals recovered for at least 30 minutes before awake trials began. After awake data collection,  
146 animals were deeply anesthetized with an intraperitoneal injection of 90 mg/kg ketamine and 9mg/kg  
147 xylazine cocktail. Data collection began approximately 10 minutes following injection.

#### 148 *Electrophysiological Signal Processing*

149 The raw data was filtered using a 2<sup>nd</sup> order Butterworth filter to produce LFP (passband 2–  
150 300 Hz) and spike streams (passband 300–5000 Hz). Common average referencing was applied to the  
151 filtered data (Ludwig et al. 2009). Multi units were identified by establishing a threshold for the high-  
152 frequency data at 3.5 standard deviations below the mean, as previously published (Kozai et al. 2012).  
153 The noise floor of the spike-stream was calculated as  $2\sigma$ , where  $\sigma$  is the standard deviation of the spike-  
154 stream over the entire recording duration after removing all threshold crossing events.

#### 155 *Data Analysis*

156 All data analysis was performed in MATLAB. Comparisons between evoked and spontaneous  
157 activity, or between brain states, were conducted on the same electrode site from the same animal.  
158 Boxplots were used to show the distribution of the data. In each boxplot, the median is represented by  
159 the horizontal line, the interquartile range is shown by the edges of the box, and the whiskers extend  
160 from the 5<sup>th</sup> to the 95<sup>th</sup> percentile. Outliers are denoted by circles and the sample mean is shown with a  
161 black X. In order to compare spontaneous and evoked activity, 64 uniformly spaced pseudo-triggers  
162 were inserted throughout the spontaneous recording epoch, similar to the spacing of visual stimuli.  
163 Evoked activity (i.e. activity following stimulus presentations) was then compared to activity following  
164 pseudo-triggers. All spectral analyses were computed using the Chronux toolbox (Bokil et al. 2010; Mitra  
165 2007) in MATLAB.

#### 166 *Analysis of Multi Unit Activity*

167 The number of multiunit threshold crossing events that occurred within a 1-second period  
168 following each stimulus presentation or pseudo-trigger was recorded. Peri-stimulus time histograms  
169 with 50ms bins were generated to show the dynamics of the multiunit response. Average multiunit  
170 firing rates were calculated using the average number of threshold crossing events within a 1-second  
171 period following each pseudo-trigger.

172 Multiunit yield is a recording performance metric that describes the functional reactivity of the  
173 surrounding tissue. Yield was defined as the percentage of electrode sites which recorded a significantly  
174 different ( $p < 0.05$ ) multiunit spike count during visual stimulation (ON condition, after stimulus onset)  
175 compared to background activity (OFF condition, before stimulus onset). To quantify evoked responses,  
176 the multiunit yield and signal to noise firing rate ratio (SNFRR) were calculated (Kozai et al. 2015b). The  
177 SNFRR (Eq. 1) compared the difference in MUA between stimulus conditions relative to the average  
178 standard deviation of each stimulus conditions:

$$179 \quad (1) \text{ SNFRR} = \frac{\mu_{ON} - \mu_{OFF}}{\frac{1}{2}(\sigma_{ON} + \sigma_{OFF})}$$

180 where  $\mu_{ON}$  and  $\mu_{OFF}$  are the mean firing rates across trials during the ON and OFF conditions, and  $\sigma_{ON}$  and  
181  $\sigma_{OFF}$  are the standard deviations of the firing rates during the ON and OFF conditions. Yield and SNFRR  
182 were parameterized by the duration of the temporal bins within the ON and OFF conditions that are  
183 being compared and the latency of each bin following stimulus onset.

#### 184 *Analysis of Local Field Potentials*

185 Negative deflections in the LFP have been shown to be correlated with neuronal firing rate and  
186 synchrony (Petermann et al. 2009). Therefore, the magnitude of synchronous LFP voltage activity was  
187 quantified using the peak-to-peak amplitude, to capture potentially relevant after-hyperpolarizations  
188 (Buzsaki et al. 2012; Kozai et al. 2015b). The sum of the full-wave rectified LFP (Kozai et al. 2015b) was  
189 also calculated as a measure of the degree to which the LFP voltage activity is temporally sustained.  
190 Calculations were performed over a 1s period following each pseudo-trigger or stimulus presentation.



191 To examine the visual stimulus' contribution to the evoked LFP response, the LFP was normalized by  
192 subtracting the spontaneous activity (amplitude or sum) from the evoked.

193 Spectral power of the LFP was calculated with the multi-taper method using a duration of 1s, a half-  
194 bandwidth of 1Hz and a taper number of 1. Relative power was measured as the ratio of the power  
195 within a specified frequency band to the broadband power (Eq. 2). Evoked power spectral densities  
196 were normalized by subtracting the log transformed spontaneous power spectrum from the log  
197 transformed evoked power spectrum (Eq. 3).

$$198 \quad (2) \quad R = \frac{\sum_a^b S(f)}{\sum S(f)}$$

$$199 \quad (3) \quad N(f) = 10 \log_{10} \left[ \frac{S_E(f)}{S_{RS}(f)} \right]$$

200 where  $R$  is relative power,  $S(f)$  is the power spectrum of the LFP,  $a$  and  $b$  are the lower and upper  
201 frequencies of the specified frequency range,  $N(f)$  is the normalized power spectrum, and  $S_E(f)$  and  $S_{RS}(f)$   
202 are the evoked and resting state power spectra respectively.

203 The laminar relationship between LFPs at different depths was quantified using the magnitude-  
204 squared coherence, which describes the similarity between two signals as a function of frequency.  
205 Coherence values range from 0 to 1, indicating either no relationship or a perfect linear relationship  
206 between signals, respectively. The coherence is given by equation 4:

$$207 \quad (4) \quad C_{xy}(f) = \frac{S_{xy}(f)}{\sqrt{S_{xx}(f)S_{yy}(f)}}$$

$$208 \quad (5) \quad \Delta C_{xy}(f) = C_{xy}^E(f) - C_{xy}^{RS}(f)$$

209 where  $C_{xy}(f)$  is the coherence,  $S_{xy}(f)$  is the cross-spectrum,  $S_{xx}(f)$  and  $S_{yy}(f)$  are the auto-spectra of the LFP  
210 from electrode sites  $x$  and  $y$  respectively. Coherence was calculated on the 1-second interval following  
211 each stimulus or pseudo-trigger, using a half-bandwidth of 3Hz and a taper number of 5, and then  
212 averaged across trials. Normalized coherence (Eq. 5) is calculated as the difference between the evoked  
213 coherence and the resting-state coherence. To assess coherence between layers, the coherence

214 between all electrode sites located within each respective layer were averaged to yield an estimate of  
215 the coherence between regions. Coherence values for specified frequency bands are given by the mean  
216 coherence within that frequency band. This estimate was then averaged across animals to compare  
217 coherence across anesthetics.

#### 218 *Assignment of cortical layers*

219 Current source density (CSD) analysis was performed by computing the second derivative of the  
220 stimulus-locked LFP voltage trace with respect to depth, and then averaged across trials. To account for  
221 a degree of uncertainty in layer assignment, putative layer IV was defined to include the two electrode  
222 sites which encompassed the location of the first evoked current sink. This first evoked current sink was  
223 defined as the minimum value of the CSD that occurred within the first 100ms following visual stimulus  
224 presentation. Given the electrode site spacing of 100 $\mu$ m, this definition describes a 'viewing distance' of  
225 approximately 300 $\mu$ m. This method has previously been verified with post-mortem histology (Kozai et  
226 al. 2014). All laminar analyses between animals were first aligned to layer IV.

#### 227 *Statistical Analysis*

228 For each comparison, normality was first assessed using the Kolmogorov-Smirnov test. If all  
229 groups were normally distributed, differences between groups were calculated using a repeated  
230 measures one-way analysis of variance (ANOVA). When one or more groups did not follow a normal  
231 distribution, a Friedman's ANOVA was performed. Post-hoc significance was confirmed using paired t-  
232 tests for normally distributed data, or Wilcoxon signed-rank tests for non-normally distributed data.  
233 Post-hoc confidence was accounted for using a Bonferroni correction.

## 234 **RESULTS**

### 235 *Spontaneous Multiunit and LFP*

236 Resting-state activity was first examined to understand how each anesthetic influences  
237 spontaneous cortical processing. Periodic bursts of multiunit activity were observed under KX anesthesia

238 (Fig. 1a), matching large deflections in the LFP (Fig. 1b). Average firing rates over one second trial  
239 durations were greater under KX compared to awake (Fig. 1c,  $p=0.01$ ;  $n=96$  electrode sites, Friedman's  
240 ANOVA), but no significant differences in firing rate were observed between anesthetics, or between  
241 isoflurane and awake. LFP peak-to-peak amplitude was significantly greater under anesthesia compared  
242 to awake ( $p<0.001$ ,  $n=96$  electrode sites, Friedman's ANOVA), and under KX compared to isoflurane  
243 ( $p=0.001$ ). LFP sum was also significantly greater under anesthesia, and under KX compared to isoflurane  
244 (Fig. 1e,  $p<0.001$ ,  $n=96$  electrode sites). It is possible that the increased LFP activity under isoflurane, in  
245 the absence of increased firing rates or bursting, may be caused by increased firing in cells located  
246 further than can be adequately resolved with multiunit recordings (Henze et al. 2000). Since the  
247 amplitude of extracellularly recorded action potentials is proportional to  $1/r^2 - 1/r$ , where  $r$  is distance  
248 from the neuronal point source (Mechler and Victor 2012; Wellman et al. 2017), a consistent increase in  
249 multiunit activity from neurons located just outside the detection range would result in recorded  
250 amplitudes just below the spike detection threshold, elevating the noise floor. Thus, to determine  
251 whether increased population activity under isoflurane anesthesia was responsible for the increases in  
252 LFP activity, despite the lack of increase in local firing rates, the noise of the spike streams was  
253 compared. Significant differences in the noise floors were not observed between brain states (Fig. 1f).  
254 The results demonstrate that KX produces synchronous bursts of multiunit activity, and both anesthetics  
255 influence the rhythmicity of ensemble activity.

#### 256 *Spontaneous oscillatory population activity*

257 To explore this further, the spectral content of the LFP was examined. Anesthetics generally  
258 produced an increase in LFP power (Fig. 2a-d,  $p<0.001$ ;  $n=96$  electrode sites, Friedman's ANOVA), but  
259 the greatest increases occurred at distinct frequencies. Isoflurane selectively increased power at alpha  
260 and beta frequencies (8-30 Hz), while KX markedly increased power at delta frequencies (2-4 Hz)(Fig.  
261 2b,e-f). Similar patterns of frequency-selective enhancement of power were observed across the depth

262 of the cortex (Fig. 2f-g). Note that although power at gamma frequencies was increased under KX  
263 anesthesia (Fig. 2b,f), the relative gamma band power was diminished (Fig 2g). These findings show that  
264 isoflurane and ketamine augment rhythmic activity at distinct frequencies.

#### 265 *Spontaneous laminar coherence*

266 Oscillatory activity is hypothesized to play an active role in facilitation of communication.  
267 Therefore, laminar LFP coherence was measured to examine the relationship between population  
268 activity at different cortical depths (Maier et al. 2010). In the awake state, coherence between  
269 supragranular (SG) and infragranular (IG) layers was slightly elevated (Fig. 3a) compared to inter-laminar  
270 coherence between different regions (e.g. granular-supragranular (G-SG) or granular-infragranular (G-  
271 IG)). However, under isoflurane anesthesia, G-IG and G-SG coherence was typically greater than SG-IG  
272 coherence (Fig. 3a-b). Averaged coherence between 7-90 Hz was significantly greater in isoflurane  
273 anesthetized mice than in awake conditions, for each pair of regions (SG-IG,  $p=0.005$ ; G-IG,  $p=0.013$ ; G-  
274 SG,  $p=0.013$ ;  $n=6$  mice, one-way ANOVA). Ketamine increased coherence slightly between all layers, but  
275 this increase was most pronounced between SG-IG regions ( $p=0.05$ ). These findings demonstrate that  
276 anesthetics influence the functional relationship between LFP activity across layers.

#### 277 *Quantification of evoked multiunit activity*

278 Having established that isoflurane and ketamine differentially influence resting-state network  
279 activity, we next asked whether evoked cortical responses differed between anesthetics. As expected,  
280 visually evoked responses demonstrate considerable temporal differences across anesthetics (Fig. 4a-b).  
281 The MU yield and signal to noise firing rate ratio (SNFRR) were compared between visual stimulation to  
282 the pre-stimulus intervals, to evaluate the responsiveness of the tissue under each anesthetic. Yield and  
283 SNFRR were calculated by comparing multiunit activity within bins, before and after the stimulus, and  
284 are therefore dependent on parameters such as bin duration and latency from stimulus onset. However,  
285 as the evoked responses demonstrated considerable temporal differences, the parameters for

286 measuring yield and SNFRR will similarly differ. To address this, the yield and SNFRR were calculated for  
287 multiple combinations of temporal bin sizes and latencies for each channel (Fig. 4b). Bin size was varied  
288 from 0.5 to 1000ms, with a temporal resolution of 0.5ms; and latency from stimulus onset was varied  
289 from 0 to 999.5ms, with a resolution of 0.5ms. MU yield and SNFRR were calculated for all combinations  
290 of bin sizes ( $B$ ) and latencies ( $L$ ) that remained within the 1s ON period, such that  $B + L \leq 1s$ . Previous  
291 studies have demonstrated that incorporating a negative latency may improve yield with periodic  
292 stimulation due to the OFF response (Kozai et al. 2015b). To explore this observation, yield and SNFRR  
293 were also calculated for all possible combinations of negative latencies ranging from 0 to 100ms, with  
294 positive latencies ranging from 0 to 200ms; and bin widths ranging from 0 to 1000ms; each with a  
295 temporal resolution of 1ms.

296 MU yield and SNFRR as a function of bin size and latency were visualized to characterize  
297 temporal differences between multiunit responses (Fig. 4c-e). Yield and SNFRR showed consistent and  
298 distinct patterns of MU dynamics between brain states. Awake animals had strong, transient responses,  
299 which were followed by a weaker, sustained response (Fig. 4c), reflecting classical visually evoked firing  
300 rate responses. In contrast, isoflurane anesthesia abolished the transient response and produced a  
301 weak, sustained response (Fig. 4d). Evoked MUA under KX demonstrates the existence of a strong  
302 transient response, and a consistent pre-stimulus burst and/or post-transient lull in MUA, followed by a  
303 rebounding increase in MUA towards the end of the stimulus period (Fig. 4e). The optimal parameters  
304 for quantifying evoked yield in each condition demonstrate that the transient response is more  
305 prolonged under KX anesthesia than awake (Fig. 4f-g). These findings suggest that isoflurane and  
306 ketamine alter the temporal dynamics of evoked multiunit responses.

### 307 *Laminar multiunit and LFP response to visual stimulus*

308 The precise number and timing of multiunit events has important implications for the  
309 representation and transmission of information. Therefore, laminar responses to the visual stimuli were

310 examined, to further explore how each anesthetic may alter the processing of visual signals. Averaged  
311 firing rates against cortical depth and time, show laminar patterns of activity that are consistent with  
312 those suggested by the previous analysis (Fig. 5a). Namely, strong transient responses are observed in  
313 awake and KX anesthetized mice, while weak, sustained responses occur under isoflurane. This weak,  
314 sustained response is limited to input layers. Additionally, periodic bursts of MUA under KX became  
315 entrained to visual stimuli, and transient responses can be observed after the start of OFF periods.  
316 Current source density analysis averaged across 64 stimuli and then across animals, shows prominent  
317 sinks across layers in awake and KX anesthetized animals, and diminished sinks across layers in  
318 isoflurane anesthetized animals (Fig. 5b). Additionally, KX anesthetized mice have a more prolonged CSD  
319 response. Evoked LFP peak-to-peak amplitude and sum in the awake mice exceeded the isoflurane  
320 response (Fig. 5c-d,  $p < 0.001$ ;  $n = 96$  electrode sites, Friedman's ANOVA), and were comparable to the  
321 ketamine response after normalization (Fig. 5e-f,  $p = 0.02$ ). These findings demonstrate that visual  
322 processing within and between layers are differentially altered by each anesthetic agent.

### 323 *Laminar coherence during visual stimulus presentation*

324         Since spatiotemporally distinct responses were demonstrated in multiunit and LFPs between  
325 isoflurane and ketamine, laminar coherence was examined to further assess the extent to which each  
326 anesthetic impaired or altered functional communication through V1. Upon visual stimulus  
327 presentation, coherence within superficial layers became elevated in awake animals (Fig. 6a). However,  
328 isoflurane did not produce large changes in coherence across depth after visual stimulus presentation.  
329 Under KX anesthesia, coherence between G-IG and G-SG layers, as well as within superficial and deep  
330 layers became elevated (Fig 6a-c). Both anesthetics had significantly greater evoked inter-laminar LFP  
331 coherence (Iso: SG-IG and G-IG  $p = 0.002$ ; G-SG,  $p = 0.003$ ; KX: SG-IG,  $p = 0.004$ ; G-IG and G-SG,  $p = 0.04$ ;  $n = 6$   
332 mice, one-way ANOVA). These findings demonstrate that both anesthetics influence the relationship  
333 between evoked population activity across layers.

### 334 *Differential responses to stimulus ON and OFF periods*

335           As a strong transient response was observed under KX during OFF periods, the evoked power in  
336 response to stimulus OFF were examined for each anesthetic, and compared to the ON response. To  
337 dissociate the effect of visual stimulation from the effects of anesthesia, evoked power was normalized  
338 by subtracting the spontaneous power spectrum from the same electrode site (Fig. 7a-d). In response to  
339 stimulus ON, the power in awake and isoflurane anesthetized mice remains relatively unchanged, with  
340 the exception of a gamma peak. This ON response peak was more prominent, and occurred  
341 approximately 10Hz slower under isoflurane (Fig. 7a,b,e). Stimulus OFF in awake animals induced a slight  
342 increase in power across cortical depth that occurred at approximately 20 Hz slower than the ON  
343 response (Fig. 7f). Similarly, in isoflurane anesthetized mice, the OFF response was more pronounced  
344 compared to awake, and occurred at approximately 20 Hz slower than the ON response (Fig. 7c,d,f). In  
345 contrast, both ON and OFF periods exhibited increased power at delta and gamma-high gamma  
346 frequencies under KX anesthesia, with no obvious ON or OFF peaks (Fig. 7e). Interestingly, although the  
347 ON and OFF periods showed distinct multiunit and oscillatory responses across anesthetics, normalized  
348 coherence across layers exhibited a similar pattern during ON and OFF periods (Fig. 8a-c). Coherence  
349 during the OFF period was greater under anesthesia (Iso: SG-IG and G-IG:  $p=0.002$ ; G-SG  $p=0.001$ ; KX:  
350 SG-IG  $p=0.004$ ; G-IG  $p=0.03$ ; G-SG  $p=0.02$ ;  $n=6$  mice, one-way ANOVA). These findings imply that the  
351 processing of visual stimuli is differentially altered between anesthetics, as ON and OFF stimuli elicit  
352 distinct oscillatory responses in awake and isoflurane anesthetized animals, while KX anesthetized mice  
353 fail to exhibit this differentiation, despite having a pronounced transient multiunit response.

### 354 **DISCUSSION**

355           This study explored the impact of anesthetic agents, isoflurane and ketamine, on spontaneous  
356 and evoked electrophysiological activity in mouse primary visual cortex. The effects of each anesthetic  
357 agent on multiunit and LFP activity were examined using intracortical electrodes. Then, coherence

358 between populations of neurons residing at different depths was measured to gain insight into the  
359 structure of communication across layers, and how this may be influenced by anesthesia. Results  
360 indicate that although isoflurane and ketamine have overlapping molecular targets, they produce  
361 distinct electrophysiological changes, which likely reflect differentially impaired signal transduction  
362 through the cortex.

### 363 *Distinct oscillatory patterns of spontaneous activity under isoflurane and ketamine anesthesia*

364 Sleep and anesthesia induce rhythmic behavior, characterized by spindle (alpha, ~7-14 Hz), delta  
365 (~1-4 Hz), and slow wave activity (~0.3 Hz) (Steriade et al. 1993a; Steriade et al. 1993b), with the  
366 emergence of slower rhythms generally indicating progression into deeper states of sleep. KX  
367 anesthetized mice exhibited pronounced delta rhythms, as well as slow, periodic bursts of multiunit  
368 activity that were likely coupled to up states during slow oscillations (Chauvette et al. 2011; Fiáth et al.  
369 2016). Isoflurane also increased delta power, but relative delta power was significantly lower than under  
370 ketamine anesthesia. Additionally, no qualitative evidence could be found for bursting multiunit activity  
371 at slow rhythms under isoflurane anesthesia. Since care was taken to avoid inducing burst suppression  
372 in the isoflurane anesthetized mice, these findings indicate that isoflurane induced animals likely had  
373 not reached the same depth of anesthesia as was achieved with ketamine/xylazine. However, this level  
374 of anesthesia was necessary in order to evoke cortical activity under isoflurane anesthesia. This  
375 difference in anesthetic depth represents an important consideration when interpreting the data.

376 In addition to the induction of delta oscillations, ketamine is known to increase and modulate  
377 power at high frequencies (Anver et al. 2011; Hakami et al. 2009; Shaw et al. 2015). Power across the  
378 gamma range and at higher frequencies showed broad increases under ketamine anesthesia. These  
379 abnormalities may stem from ketamine's primary action as an NMDA receptor antagonist. NMDAR  
380 antagonists preferentially inhibit GABAergic interneurons, causing disinhibition, or aberrant excitation



381 (Brown et al. 2011; Homayoun and Moghaddam 2007). Accordingly, spontaneous firing rates increased  
382 under ketamine anesthesia.

383         Although isoflurane also inhibits NMDA receptors and decreases cortical inhibition (Haider et al.  
384 2013), no significant differences in spontaneous firing rates could be identified under isoflurane  
385 anesthesia compared to awake animals. This may be due to isoflurane's potentiation of GABA<sub>A</sub>  
386 receptors and inhibition of AMPA receptors (Alkire et al. 2008). GABA<sub>A</sub> receptors are prevalent  
387 throughout the cortex and their potentiation results in widespread hyperpolarization of pyramidal  
388 neurons (Bai et al. 1999; Brown et al. 2011; Garcia et al. 2010; Sigel and Steinmann 2012). AMPA  
389 receptors are glutamatergic post-synaptic receptors, which, in the visual cortex, facilitate excitatory  
390 feedforward activity (Self et al. 2012; van Kerkoerle et al. 2014).

391         Despite the lack of an increase in firing rate, resting-state LFP activity and broadband power  
392 increased under isoflurane anesthesia, demonstrating that isoflurane increases the rhythmicity of  
393 ensemble activity. A previous examination of resting-state activity in ferret V1 under isoflurane/xylazine  
394 anesthesia, found that anesthesia did not increase broadband power in visual cortex (Sellers et al. 2013).  
395 The reason for this discrepancy is unclear, but may be related to the use of xylazine.  $\alpha$ 2-adrenergic  
396 agonists, such as xylazine, decreased firing rates of spontaneous and visually driven cells in rat visual  
397 cortex (Kolta et al. 1987), and decreased gamma band power in the olfactory bulb (Chery et al. 2014).  
398 Interestingly, relative power under isoflurane anesthesia was greatest, compared to the other two  
399 groups, within alpha and beta frequency bands (7-30 Hz).

#### 400 *Functional implications for oscillatory dynamics*

401         Neuronal oscillations may play an important role in mediating communication between neurons  
402 and cortical regions. In this regard, slow rhythms are typically thought to obstruct communication. For  
403 example, large amplitude, hypersynchronous slow waves during sleep and anesthesia are thought to  
404 disrupt the processing and communication of information, and thus be related to loss of consciousness

405 (Franks 2008). Similarly, frontal alpha hypersynchrony disrupts communication between brain regions  
406 and occurs concomitantly with loss of consciousness (Cimenser et al. 2011; Supp et al. 2011). In visual  
407 cortex, alpha rhythms may be associated with active suppression of information processing (Klimesch et  
408 al. 2007; Worden et al. 2000) and gamma rhythms with feature encoding and attention (Fries et al.  
409 2001; Singer and Gray 1995). However, the functional role of gamma rhythm is subject to debate (Cardin  
410 2016; Fries 2009; Jia et al. 2011; Ray and Maunsell 2010; 2015). Nevertheless, gamma oscillations reflect  
411 intrinsic properties of network activity, and are associated with GABA<sub>A</sub> receptor mediated inhibition, and  
412 fast-spiking parvalbumin-expressing (FS PV) inhibitory interneurons (Buzsáki and Wang 2012; Carlen et  
413 al. 2012). Evoked responses to stimulus ON and OFF periods elicited pronounced gamma oscillations  
414 under isoflurane anesthesia, which occurred at lower frequencies, than awake. This might be due to  
415 isoflurane's potentiation of the GABA<sub>A</sub> receptor, which prolongs the deactivation time of the GABA-  
416 induced current, and may thus decrease the frequency of the evoked gamma oscillation (Bai et al. 1999;  
417 Brunel and Wang 2003; Wang and Buzsáki 1996).

418         Interestingly, OFF periods in both awake and isoflurane anesthetized states demonstrated a  
419 consistently slower gamma response than was evoked during ON periods. Gamma oscillation frequency  
420 in V1 has been shown to be sensitive to contrast (Ray and Maunsell 2010). However, to our knowledge,  
421 distinct and consistently induced gamma oscillations have not been observed in response to contrast-  
422 OFF stimuli. Another possible origin for this response might be the luminance decrement associated  
423 with the stimulus turning off. Light and dark stimuli are processed through separate pathways in the  
424 retina and thalamus, but within the cortex, the segregation of these signals is less clearly understood.  
425 Asymmetries in cortical neuronal response properties between light and dark stimuli have been  
426 observed (Kremkow et al. 2014), and recent work has identified small groups of neurons in layer II/III  
427 that respond strongly to either ON or OFF stimuli (Smith et al. 2015). Perhaps these distinct oscillatory  
428 responses reflect differences in excitatory/inhibitory responses to contrast or luminance decrements.

429 However, the physiological mechanism underlying this response is currently unclear and can be explored  
430 more systematically in future work.

#### 431 *Differential effects of isoflurane and ketamine on laminar communication*

432 A pattern of highly coherent, intra-laminar spontaneous activity under isoflurane anesthesia was  
433 observed, with relatively weak SG-IG coherence, compared to G-IG or G-SG. This pattern contrasts with  
434 that of the awake or ketamine anesthetized mice, which exhibited comparable or slightly elevated SG-IG  
435 coherence (compared to G-IG or G-SG coherence) and suggests that isoflurane alters the communicative  
436 relationship between layers. Visually evoked multiunit responses were diminished and temporally  
437 sustained in layer IV under isoflurane anesthesia. Correspondingly, evoked LFP peak-to-peak amplitude  
438 was generally smaller than spontaneous, indicating that rhythmic baseline activity was disrupted by  
439 visual stimulation in such a way that decreased the synchronicity of ensemble activity. Pronounced  
440 current sinks observed in layers IV and II/III, and weaker sinks seen in layer V, further suggest that  
441 isoflurane disrupts the temporal organization of visual stimulus induced local field potentials. Following  
442 visual stimulation, laminar coherence remained significantly elevated compared to awake, and exhibited  
443 only slight changes in coherence compared to spontaneous activity.

444 Ketamine was also shown to increase resting-state coherence between layers. However, the  
445 pattern of coherence between and within layers under ketamine anesthesia remained similar to that of  
446 awake animals. Visually evoked multiunit yield and optimal bin sizes to measure yield, were each greater  
447 under ketamine anesthesia than awake, suggesting that the transient response was both more  
448 pronounced and sustained. Additionally, visual stimuli appear to have entrained spontaneous bursting  
449 multiunit activity, such that bursts coincide temporally with stimulus changes (OFF-ON and ON-OFF),  
450 thereby maximizing neuronal responsiveness (Hasenstaub et al. 2007; Shu et al. 2003). Robust current  
451 sinks in layers IV, II/III and V suggest effective signal propagation across the cortex. Laminar coherence  
452 increased after visual stimulation within superficial and deep layers, as well as between regions, even at

453 higher frequencies. As gamma coherence is spatially restricted (Jia et al. 2011), this may reflect  
454 functional communication between anatomical connections (Douglas and Martin 2004; Hirsch and  
455 Martinez 2006). Taken together, the data suggests that isoflurane anesthesia suppressed while  
456 ketamine enhanced laminar communication in V1.

#### 457 *Conclusion*

458         The chronic nature of this experiment introduces the possibility for confounds, such as electrode  
459 failure (Barrese et al. 2013; Wellman et al. 2017), altered neuronal gene expression following chronic  
460 exposure to isoflurane (Kaneko et al. 2005), or changes in visual response properties due to age related  
461 changes to visual cortex physiology (Mendelson and Wells 2002; Polidori et al. 1993). However, since  
462 direct pairwise comparisons were made within animals, these experimental confounds were minimized.  
463 Additionally, 8-9 month old mice are not expected to exhibit significantly different changes in visual  
464 acuity or contrast sensitivity than younger mice (Lehmann et al. 2012).

465         Our results indicate that although isoflurane and ketamine share numerous molecular targets,  
466 they exhibit distinct spontaneous network behaviors and differentially alter laminar processing in visual  
467 cortex. These findings demonstrate that different anesthetics may present different circuit level  
468 electrophysiological behaviors, which may be an important consideration for studies that draw  
469 physiological conclusions from experiments on anesthetized animals. Further comparative analyses  
470 should therefore be conducted in this area to characterize dose dependent changes in laminar activity  
471 across a more exhaustive list of anesthetic regimes. For example, urethane is a widely used anesthetic  
472 agent for acute neurophysiological studies, and further analysis in this regard will provide important  
473 information for future studies. This type of analysis may ultimately allow for a more careful selection of  
474 appropriate anesthetic agents. Additionally, these differences may provide insight into how perturbed  
475 network activity contributes to altered brain states during unconsciousness or as a result of neurological  
476 disorders.

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482 **DISCLOSURES**

483 No conflicts of interest, financial or otherwise, are declared by the authors.

484 **AUTHOR CONTRIBUTIONS**

485 T.D.Y.K. and N.J.M. conception and design of research; T.D.Y.K. performed experiments; N.J.M. analyzed  
486 data; N.J.M. and T.D.Y.K. interpreted results of experiments; N.J.M. prepared figures and drafted  
487 manuscript; N.J.M. and T.D.Y.K. edited and revised manuscript, and approved final version of  
488 manuscript.

489 **Figure Captions**

490

491 Figure 1: Anesthetics alter temporal aspects of resting state population activity. a) Representative spike  
492 streams recorded from layer IV in the same animal at the same electrode site. MUA under ketamine  
493 anesthesia exhibits bursting characteristics. b) LFPs corresponding to spike streams from (a). Large,  
494 negative deflections in the ketamine example match bursts in the MUA. c) Average firing rates along the  
495 length of the electrode shank, computed over one second intervals, were slightly greater under  
496 ketamine anesthesia. Amplitude of the noise floor did not differ significantly across anesthetics. d-e) LFP  
497 peak to peak amplitude and sum are significantly greater under anesthesia. Ketamine has significantly  
498 greater LFP activity than isoflurane. f) Amplitude of the noise floor did not differ significantly across  
499 anesthetics. (n=96 electrode sites: \* p<0.001, # p=0.001, % p=0.01)

500

501 Figure 2: Isoflurane and ketamine increase resting-state power at distinct frequencies. a) Representative  
502 power spectra, recorded from layer IV in the same animal at the same electrode site. b) Power spectra  
503 from (a), normalized by subtracting the awake spectrum from the anesthetized. c-d) Anesthesia  
504 significantly increases mean and peak power, along the depth of the cortex. e) Awake induced LFP  
505 power against depth, averaged across pseudo-triggers, and then animals. Depth is relative to layer IV,  
506 indicated by the dotted black regions. f) Averaged power against depth under isoflurane and ketamine  
507 anesthesia, normalized to awake, as in (b). Largest increases in power occur at alpha and beta  
508 frequencies under isoflurane, and delta and gamma frequencies under ketamine. g) Relative power  
509 within frequency bands are differentially affected by isoflurane and ketamine. (n=96 electrode sites: \*  
510  $p < 0.001$ , #  $p = 0.002$ )

511

512 Figure 3: Resting state coherence increases under anesthesia. a) Mean pairwise coherence across  
513 electrode sites for awake, isoflurane anesthetized, and ketamine anesthetized animals. Each cell  
514 represents the mean coherence between two electrode sites, averaged across pseudo triggers and  
515 animals. Cells along the diagonal show the average coherence between signals recorded from the same  
516 electrode site, and are thus equal to one. Dotted black regions indicate layer IV. White rectangles border  
517 supragranular-infragranular (SG-IG), granular-infragranular (G-IG), and granular-supragranular (G-SG)  
518 regions. b) Laminar SG-IG, G-IG, and G-SG coherence against frequency. Interlaminar coherence for each  
519 animal was calculated as the average coherence in each region. Bold lines indicate the mean coherence  
520 across animals, and dim lines indicate standard error. Shaded regions encompass alpha, beta, and  
521 gamma frequency bands and are used in the calculations for (c). c) Mean coherence between 7-90 Hz,  
522 averaged across animals. Error bars denote standard error. (n=6 mice: \*  $p < 0.05$ )

523

524 Figure 4: Quantification of evoked multiunit activity. a) Representative peri-stimulus time histograms of  
525 evoked responses, recorded from layer V. Each row shows examples from the same mouse at the same  
526 electrode site across anesthetics. Evoked responses exhibit dynamic temporal variability across  
527 anesthetics. b) Example diagram for how multiunit yield was calculated. MUA was quantified by  
528 comparing spike counts,  $X_s$ , within a bin of duration,  $B$ , at some latency,  $L$ , after each stimulus. This  
529 distribution of spike counts was then compared to the spike counts within the same bin duration, at  
530 some latency,  $L'$ , before stimulus presentation, using a paired t-test. Analysis was repeated for varying  
531 bin sizes and latencies to capture dynamic changes in the evoked response, and then performed on all  
532 channels and all animals. c-e) Pseudo-color plots demonstrate the resultant MU yield and signal to  
533 noise firing rate ratio (SNFRR, insets). For ease of visualization, all plots show negative latency ( $L'$ ) equal  
534 to 0, such that all bin sizes and post-stimulus latencies are compared with the same duration  
535 immediately before the stimulus. Awake animals have a consistent, strong transient response, followed  
536 by ~100ms of slightly elevated MUA. Alternatively, isoflurane anesthetized animals do not produce a  
537 strong transient response, and firing rates are only slightly elevated compared to pre-stimulus intervals.  
538 Ketamine anesthesia produces a strong transient response, but periodic bursts of MUA are still observed  
539 in the pre-stimulus interval (Fig a, e). Note that the negative SNFRR indicates that firing rates during the  
540 pre-stimulus interval exceeded those in the post-stimulus interval, for the parameters specified by  $B$  and  
541  $L$ . f-g) Parameter values that optimized multiunit yield are shown without the negative latency  
542 parameter, as in c-e (f), and with the negative latency parameter (g).

543

544 Figure 5: Laminar responses to visual stimulus further demonstrate temporal variability. a) Multiunit  
545 firing rate across depth and time, averaged across 64 stimuli, and then across animals. Stimulus  
546 presentation is shown by gray bar. Strong transient responses are observed in awake and ketamine  
547 anesthetized mice. Isoflurane reduces the temporal synchrony and prolongs the evoked response.

548 Bursting MUA observed in the spontaneous condition under ketamine anesthesia are apparent in the  
549 visually evoked response. b) Induced current source densities, averaged across 64 stimuli, and then  
550 across animals. Awake animals demonstrate succinct laminar processing, compared to ketamine.  
551 Isoflurane CSD is the weakest and shortest. c-f) Quantification of LFP shows synchronous population  
552 activity in the awake case (c-d), and synchronous and sustained population activity under ketamine (c-f).  
553 Isoflurane exhibits a weak evoked response. (n=96 electrode sites: \* p<0.001, % p=0.02)

554

555 Figure 6: Visually evoked laminar coherence increases under anesthesia. a) Normalized pairwise  
556 coherence, measured as the difference between coherence during ON periods and spontaneous  
557 coherence, for awake, isoflurane anesthetized, and ketamine anesthetized animals. b) Evoked SG-IG, G-  
558 IG, and G-SG coherence (mean  $\pm$  standard error) against frequency. Coherence for each animal was  
559 calculated as the average coherence in each region encompassed by the white borders in (a). c) Mean  
560 coherence between 7-90 Hz (shaded region in (b)), averaged across animals. Error bars denote standard  
561 error. (n=6 mice: # p<0.05, \* p<0.01)

562

563 Figure 7: Anesthetics alter rhythmic properties of the evoked response. a) Representative power spectra  
564 recorded from layer V, at the same electrode site in the same mouse. Spontaneous power spectra at the  
565 same electrode site are shown as dotted lines. Broadband increases in power are observed under  
566 anesthesia. b) Power spectra in (a), normalized by subtracting the spontaneous power spectrum from  
567 the evoked. A pronounced, visually evoked gamma peak is observed under isoflurane, at slower  
568 frequencies than awake. Largest increases in power after visual stimulation under ketamine occur at  
569 delta frequencies and across high frequencies. c-d) Anesthesia significantly increases power across the  
570 depth of the cortex. e) Power across the depth of the cortex, averaged across 64 stimuli, and then across  
571 animals, normalized to resting state as in (b).



572

573 Figure 8: Evoked OFF response has similar structure of laminar coherence as ON response. a) Normalized  
574 pairwise coherence changes during OFF periods for awake, isoflurane anesthetized, and ketamine  
575 anesthetized animals. b) Coherence (mean  $\pm$  standard error) between SG-IG, G-IG, and G-SG layers. c)  
576 Average coherence from 7-90 Hz, averaged across animals. Error bars indicate standard error. (n=6  
577 mice: \* p<0.05)

578

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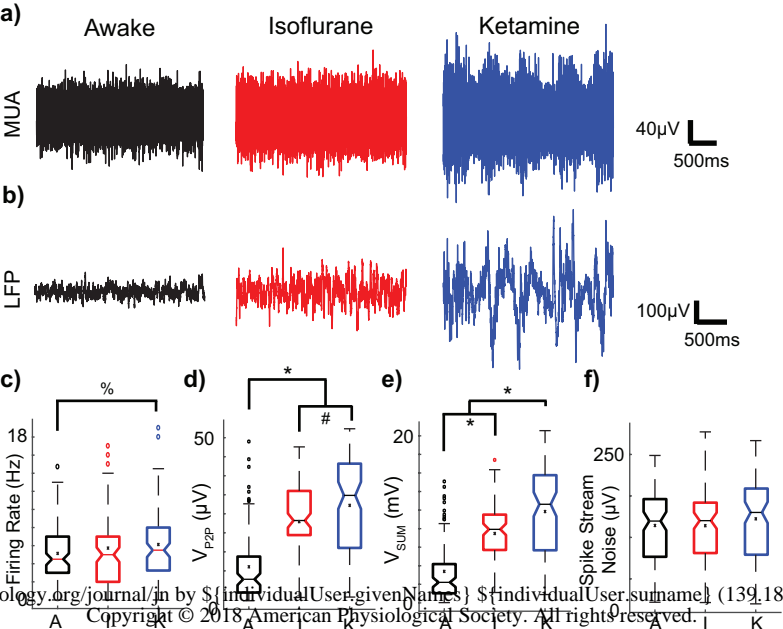
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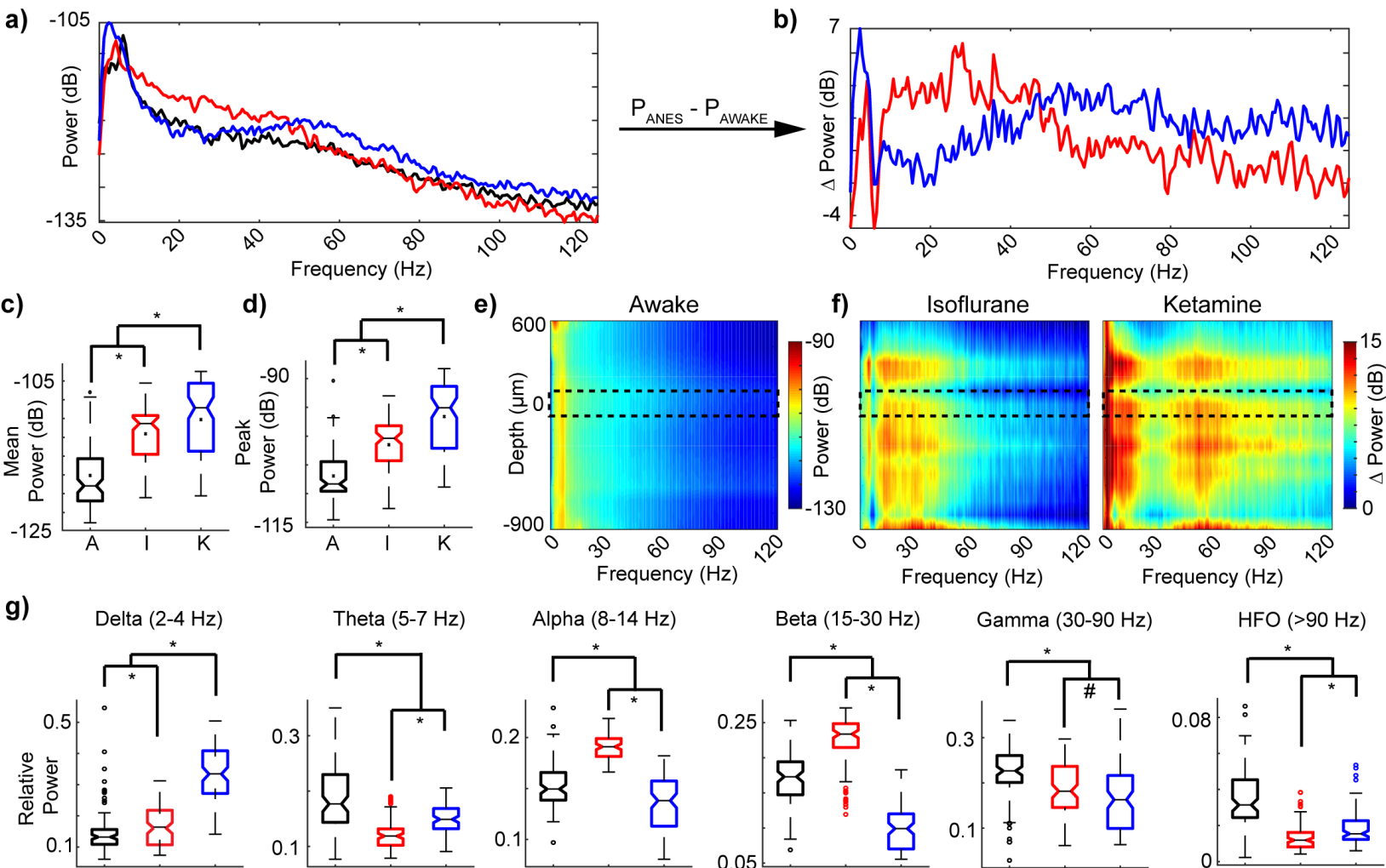
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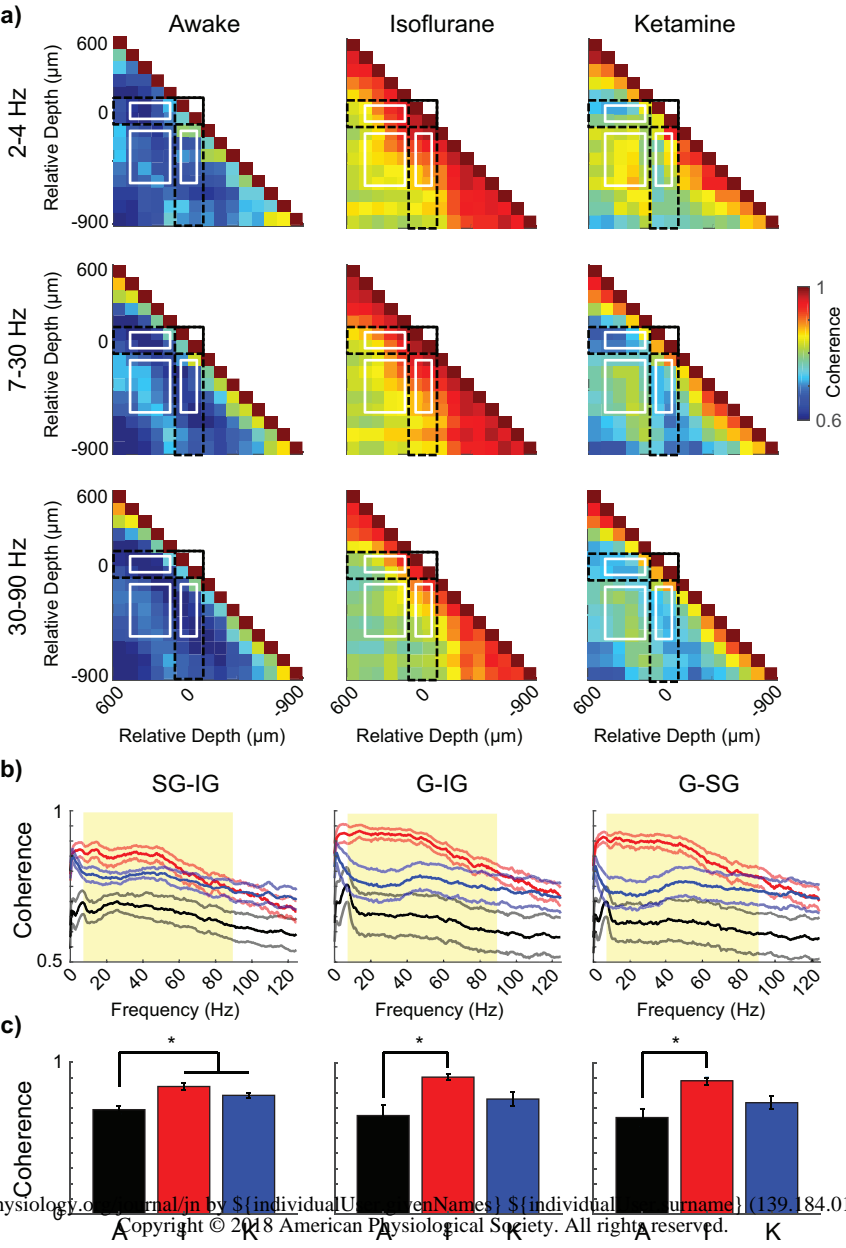
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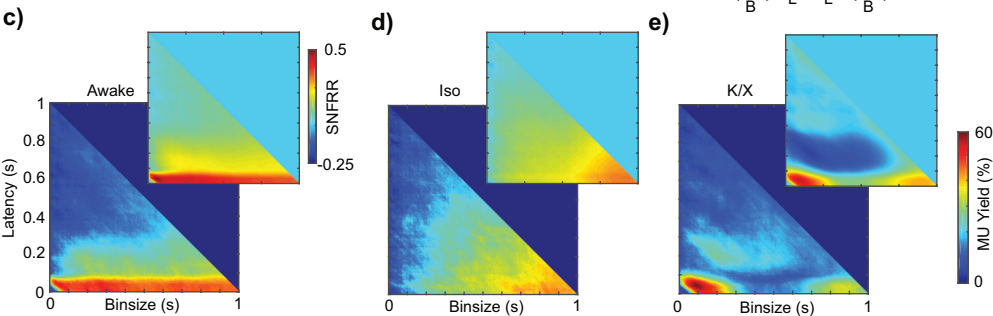
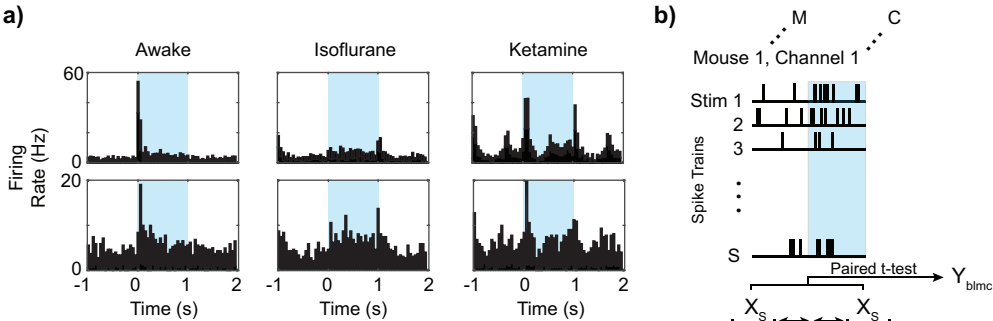
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**f)**

	B (ms)	L (ms)	L' (ms)	Yield (%)	SNFRR
Awake	66.5	30.5	0	54.0	0.49
Iso	840.5	18.0	0	45.8	0.31
K/X	101.5	38.5	7	60.2	0.44

**g)**

	B (ms)	L (ms)	L' (ms)	Yield (%)	SNFRR
Awake	59	39	15	56.3	0.47
Iso	835	21	59	50	0.31
K/X	94	38	7	60.2	0.44

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